Role of exponential apparent diffusion coefficient in characterizing breast lesions by 3.0 Tesla diffusion-weighted magnetic resonance imaging

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Abstract

Objective: To evaluate the role of exponential apparent diffusion coefficient (ADC) as a tool for differentiating benign and malignant breast lesions.

Patients and Methods: This prospective observational study included 88 breast lesions in 77 patients (between 18 and 85 years of age) who underwent 3T breast magnetic resonance imaging (MRI) including diffusion-weighted imaging (DWI) using b-values of 0 and 800 s/mm² before biopsy. Mean exponential ADC and ADC of benign and malignant lesions obtained from DWI were compared. Receiver operating characteristics (ROC) curve analysis was undertaken to identify any cut-off for exponential ADC and ADC to predict malignancy. P value of <0.05 was considered statistically significant. Histopathology was taken as the gold standard.

Results: According to histopathology, 65 lesions were malignant and 23 were benign. The mean ADC and exponential ADC values of malignant lesions were 0.9526 ± 0.203 × 10⁻³ mm²/s and 0.4774 ± 0.071, respectively, and for benign lesions were 1.48 ± 0.4903 × 10⁻³ mm²/s and 0.317 ± 0.1152, respectively. For both the parameters, differences were highly significant (P < 0.001). Cut-off value of ≤0.0011 mm²/s (P < 0.0001) for ADC provided 92.3% sensitivity and 73.9% specificity, whereas with an exponential ADC cut-off value of >0.4 (P < 0.0001) for malignant lesions, 93.9% sensitivity and 82.6% specificity was obtained. The performance of ADC and exponential ADC in distinguishing benign and malignant breast lesions based on respective cut-offs was comparable (P = 0.109). Conclusion: Exponential ADC can be used as a quantitative adjunct tool for characterizing breast lesions with comparable sensitivity and specificity as that of ADC.

Key words: Apparent diffusion coefficient; breast MRI; diffusion-weighted imaging; exponential apparent diffusion coefficient

Introduction

High field strength (3T) magnetic resonance imaging (MRI) is now increasingly being used for detection and diagnosis of breast lesions due to its better spatial resolution, higher signal-to-noise ratio (SNR), and shorter image acquisition time. Though dynamic contrast-enhanced MRI (DCE-MRI) has high sensitivity, its relative low specificity and low positive predictive value in...
Distinguishing malignant and benign breast lesions causes unnecessary biopsies.[3] Diffusion-weighted imaging (DWI) is a noncontrast, functional MRI sequence that has shown promise in increasing DCE-MRI specificity.[4,5]

DWI is a fat-saturated T2-weighted spin echo prepared echo planar image sequence with diffusion gradients applied before and after the 180 degree pulse.[6] DWI may be acquired for several (minimum of two) b values, where b determines the degree of diffusion weighting; apparent diffusion coefficient (ADC) is then calculated by using the formula “S = $S_0 \times \exp(-b \times \text{ADC})” where S is the signal intensity after application of the diffusion gradient and $S_0$ is the signal intensity on the diffusion image acquired at $b = 0 \text{ s/mm}^2$.[3,4] At low b-value, the contribution of perfusion to the ADC is higher than diffusion effects.[7,8] At higher b-values, only diffusion effect remains, increased contrast resolution is achieved but at the expense of SNR.[5,9]

DWI measures the water molecules mobility (Brownian motion) in vivo on unenhanced MRI sequences and noninvasively evaluates tissue biophysical characteristics such as cell density, membrane integrity, and extracellular matrix composition.[10] The image contrast in DWI is determined by the random microscopic motion of the water molecules with low diffusibility of water molecules corresponding to lower signal loss and hypointense areas; high diffusion corresponds to a higher signal loss and hypointense areas.[11] However, the signal intensity of DWI is also influenced by the intrinsic T2 properties of the tissue being examined along with water diffusibility; therefore, benign lesions with high intrinsic T2 signal intensity can also appear bright on DWI because of the T2 “Shine-Through” effect.[12] This T2 shine-through effect can be eliminated by generating ADC map from two or more DWI sets and exponential ADC images which depends only on the diffusion of water molecules but also on T2 signal characteristics.[12] ADC is a quantitative measure directly proportional to water diffusion.[13] Increased cellular density in malignant lesions compared to benign lesions and normal breast tissue results in decreased space for extracellular water diffusion and renders these lesions hyperintense on DWI and hypointense on ADC maps.[9,10] The exponential ADC image is obtained on a workstation using the formula $S_b/S_0 = \text{Exponential ADC} = \exp\left(-b \times \text{ADC}\right)$, where b stands for the b value of the DWI sequence (i.e., $b = 800 \text{ s/mm}^2$ in our study), and $S_b$ and $S_0$ are the signal intensities on the diffusion-weighted image and the reference image, respectively.[12,14] In case of true diffusion restriction, the exponential ADC images retain the hyperintense signal as seen on DWI while T2 shine through images are isointense, thus improving tissue contrast and eliminating the T2 shine through effect.[12,14,15] DWI has its limitations too. It is more prone to susceptibility artefacts and image distortion making characterization of small lesions difficult.[2,4]

Our study aims to evaluate the role of exponential ADC as a tool for differentiating benign and malignant breast lesions.

**Patients and Methods**

**Study population**

This is a prospective observational study conducted in the Department of Radio-diagnosis in collaboration with the Department of General Surgery and Department of Pathology of IPGME and R-SSKM Hospital, Kolkata. The study was approved by the “Institutional Ethical Committee”. Seventy-seven women with 88 suspicious breast lesions who underwent MR mammogram in our hospital between January 2015 and May 2016 were included in the study.

**Inclusion criteria**

Female patients with suspicious breast lesions assessed by clinical/physical examination and/or ultrasonography and/or mammography.

**Exclusion criteria**

- Less than 1 cm contrast enhancing masses
- Previous or current neoadjuvant or radiation therapy
- Previous interventional or surgical procedures in the 3 months preceding the examination
- Male patients presenting with breast lumps
- Patients without histopathological confirmation of the breast lesion
- Patients who had general contraindications to MRI were excluded such as:
  - Patients having history of allergic manifestation to contrast or other drug
  - Patients with implanted cardiac pacemaker, aneurysm clips, cochlear, or other such devices contraindicated for MRI examination
  - Patients having claustrophobia
  - Unwillingness to be a part of the study.

All the patients signed a written informed consent form in their own local language followed by history taking and general and local examination. MRI was done during the second week of menstrual cycle for premenopausal women. MRI included both DCE and DWI sequences.

**MRI acquisition and postprocessing**

Bilateral breast MRI was performed using 3.0T MR (Signa HDx 3.0T, GE Medical Systems) with a dedicated 16-channel bilateral breast coil with patient in the prone position. Bilateral breast MRI was done using the following protocol – an axial T2 sequence (TR/TE 3300/85; slice thickness 4 mm without any interslice gap; field of view (FOV) 32 × 32; matrix size 288 × 256); an axial STIR sequence (TR/TE 3125/68; inversion time 175 ms; slice thickness 4 mm without any interslice gap; FOV 32 × 32;
matrix size 288 × 192); echo planar imaging (EPI)-based DWI sequence in axial planes at b values of 0 and 800 s/mm² (TR/TE 5825/minimum; slice thickness 4 mm; interslice gap 0; FOV 32 × 32 and matrix size 96 × 140; bandwidth 125 kHz; number of excitation 16; acquisition time 4–5 min depending on number of slices); an axial VIBRANT multiphase three-dimensional (3D) T1-weighted dynamic gradient-echo sequence obtained after 10 ml intravenous bolus injection of gadolinium DTPA at a rate of 2.5 ml/s followed by a 20-ml saline flush (flip angle 12°; slice thickness 2 mm with no interslice gap; FOV 36 × 36; matri × 320 × 320). Dynamic study comprised one precontrast and 7 postcontrast series, each phase lasting 1 min 21 s. Automated subtracted images were obtained for each of the seven phases. Kinetic curve assessment of the fastest enhancing component of the lesion or the most suspicious curve pattern in the lesion was assessed with the available software (Functool) in GE Workstation.

MRI interpretation
Lesions were assigned BI-RADS value based on DCE morphologic and kinetic curve features. DWI were obtained before DCE-MRI. A radiologist with 10 years of experience in MRI measured ADC and exponential ADC values. Region of interest (ROI) was placed on slice with the largest diameter showing the highest signal intensity on DWI image. ROI was automatically placed in the exponential ADC and ADC maps corresponding to the selected ROI in the DWI image by the “Functool” software. ROI did not include cystic, hemorrhagic, or necrotic areas. Size of ROI was not fixed and it varied according to the size of the area showing diffusion restriction. The ADC and exponential ADC values were calculated by the “Functool” software. The lesions showing varied ADC and Exponential ADC values, the lowest ADC and the corresponding exponential ADC value was taken into calculation.

Reference standard
All lesions with a MR BI-RADS category 3, 4, or 5 were ascertained with surgically excised specimen (n = 70) or with 14-gauge core needle biopsy under ultrasound (n = 18). Histopathological diagnosis was taken as the gold standard.

Statistical analysis
Data have been summarized as mean and standard deviation for numerical variables. Normality was tested by Kolmogorov–Smirnov goodness-of-fit test to a normal distribution, and age, ADC, and exponential ADC data showed normal distribution. They were compared between benign and malignant subgroups by Student’s independent samples t-test. P < 0.05 was considered to be statistically significant. ROC curve analysis was undertaken to identify any cut-off for ADC or exponential ADC to predict malignancy. The performance of ADC and exponential ADC in distinguishing between benign and malignant breast lesions based on respective cut-offs were compared by McNemar’s Chi-square test. The extent of agreement between individual diagnostic parameters and the gold standard diagnosis of histopathology was estimated as Cohen’s kappa with its 95% confidence interval. MedCalc version 11.6 (Mariakerke, Belgium: MedCalc Software 2011) and Statistica version 6 (Tulsa, Oklahoma: StatSoft Inc., 2001) software were used for the analysis.

Results
Seventy-seven women (between 18 and 85 years of age, mean age 67 years) with 88 breast lesions were included in the study, of which 65 were malignant and 23 were benign [Figure 1]. The mean age of women with malignant breast lesions was 48.1 years (age range 22–85 years; standard deviation 12.7) and for benign it was 36.2 years (age range 18–49 years; standard deviation 9.04). The mean size of ROI was 77.63 mm² (range 46.8–118.4 mm²; standard deviation 19.42). According to the final histopathology the malignant lesions were – invasive ductal carcinoma (n = 47) [Figure 2], invasive ductal carcinoma with ductal carcinoma in situ (n = 3), inflammatory intraductal carcinoma (n = 8), pure mucinous carcinoma (n = 1), mixed mucinous carcinoma (n = 1), infiltrating lobular carcinoma (n = 1), invasive papillary carcinoma (n = 1), malignant phyllodes (n = 1), and invasive metaplastic carcinoma (n = 2), while the benign lesions included fibroadenoma (n = 4), idiopathic granulomatous mastitis (n = 5), benign phyllodes (n = 1), fibrocystic disease of breast (n = 4), fibroadenolipoma (n = 2), benign proliferative lesion (n = 1), ductal adenoma (n = 2), tubular adenoma (n = 1), hyalinized fibroadenoma (n = 1) [Figure 3], fibroadenosis with epitheliosis (n = 1), and intraductal papilloma (n = 1).

Statistically significant difference was observed between the mean exponential ADC and ADC values of benign and malignant lesions. The mean ADC and exponential ADC values of malignant lesions were 0.9526 ± 0.203 × 10⁻³ mm²/s
and 0.4774 ± 0.071, respectively, and for benign lesions were 1.48 ± 0.49 × 10⁻³ mm²/s and 0.317 ± 0.115, respectively. For both the parameters, differences were highly significant (P < 0.001).

ROC curve analysis [Figure 4] suggested that ADC ≤1.1 × 10⁻³ mm²/s indicates the possibility of malignancy in the breast lesion with 92.3% (95% CI 83.0–97.5) sensitivity and 73.9% specificity (95% CI 51.6–89.8); when ROC was higher than 0.4 [Figure 5], sensitivity and specificity of exponential ADC value of malignancy were 93.9% (95% CI 85.0–98.3) and 82.6% (95% CI 61.2–95), respectively.

The performance of ADC and exponential ADC in distinguishing between benign and malignant breast lesions based on the respective cut-offs was compared by McNemar’s Chi-square test which showed the two modalities to be comparable (P = 0.109).

The strength of agreement when compared between individual diagnostic parameters (ADC, exponential ADC) and the gold standard diagnosis of histopathology estimated as Cohen’s kappa with its 95% confidence interval were better with exponential ADC [Tables 1 and 2]. Kappa statistics is derived as measure of agreement (adjusted against the proportion of disagreement) and in this case has been calculated from cut-off derived from the ROC. Therefore, the sensitivity and specificity obtained through the ROC analysis is reported.

Table 1: Cross-tabulation of diagnosis by ADC cut-off vis-a-vis the gold standard histopathological diagnosis: With extent of agreement depicted as Cohen’s Kappa

<table>
<thead>
<tr>
<th>Histopathological diagnosis (gold standard)</th>
<th>Status ADC</th>
<th>Row total (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Benign</td>
<td>Benign</td>
<td>17 (30.7%)</td>
</tr>
<tr>
<td>Malignant</td>
<td>Malignant</td>
<td>55 (69.3%)</td>
</tr>
<tr>
<td>Column total (%)</td>
<td></td>
<td>88 (100%)</td>
</tr>
</tbody>
</table>

Kappa: 0.554
Standard error: 0.0980
95% CI: 0.362-0.746

Interpretation: Good agreement between the two modalities

Table 2: Cross-tabulation of diagnosis by Exponential ADC cut-off vis-a-vis the gold standard histopathological diagnosis: With extent of agreement depicted as Cohen’s Kappa

<table>
<thead>
<tr>
<th>Histopathological diagnosis (gold standard)</th>
<th>Status Exponential ADC</th>
<th>Row total (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Benign</td>
<td>Benign</td>
<td>19 (26.1%)</td>
</tr>
<tr>
<td>Malignant</td>
<td>Malignant</td>
<td>61 (73.9%)</td>
</tr>
<tr>
<td>Column total (%)</td>
<td></td>
<td>88 (100%)</td>
</tr>
</tbody>
</table>

Kappa: 0.765
95% CI: 0.610-0.919

Interpretation: Strong agreement between the two modalities

Figure 2 (A-G): 40 year old woman with invasive ductal carcinoma in right breast. Axial DWI (b 800s/mm²) shows tumor as high signal intensity in both DWI and EXPONENTIAL ADC map images (A and C respectively) and low signal intensity in ADC map image (B). ADC and EXPONENTIAL ADC values were 0.000926 mm²/s and 0.479 respectively. An irregularly marginated hypointense lesion is seen on T2WI (D) with heterogenous enhancement on post-contrast study (E). (F) (H&E 10X10) and (G) (H&E 40X10)-Section shows infiltration of stroma by cords and nests of pleomorphic malignant ductal cells.
In our study, we evaluated the role of exponential ADC and ADC in distinguishing benign and malignant breast lesions at b-value of 800 s/mm². To our knowledge, this is the first study to calculate the mean exponential ADC and cut-off value for differentiating benign and malignant breast lesions. No additional sequence is required for interpretation of exponential ADC, thus saving time. The mean exponential ADC values for malignant and benign lesions were 0.4774 and 0.317, respectively. The mean ADC value of malignant lesions was 0.9526 ± 0.203 × 10⁻³ mm²/s and that for benign lesions was 1.48 ± 0.49 × 10⁻³ mm²/s. These values are in agreement with the results of previous studies by Woodhams et al., Abdulghaffar et al., Park et al., Bansal et al., Palle et al., and Kul et al.

The cutoff values for ADC and exponential ADC derived from ROC analysis were 1.1 × 10⁻³ mm²/s and 0.4, respectively, for predicting malignancy. Fifty-five lesions of the 65 malignant and 17 of the 23 malignant lesions were classified correctly using the ADCs, resulting in 92.3% sensitivity and 73.9% specificity; whereas 61 out of 65 malignant lesions and 19 out of 23 benign lesions were correctly classified using the exponential ADC cutoff of 0.4, resulting in higher sensitivity and specificity (93.9% and 82.6%, respectively).

Six lesions were false positive, as suggested by ADC. These lesions include four cases of idiopathic granulomatous mastitis, one case of fibroadenosis with epitheliosis and one case of fibrocystic disease of the breast. The mean ADCs of idiopathic granulomatous mastitis (mean 0.9132 × 10⁻³ mm²/s, range 0.632–1.15 × 10⁻³ mm²/s) is significantly lower than those of benign lesions. Similarly the mean exponential ADC value for idiopathic granulomatous mastitis (0.4886, range 0.4–0.604) were higher than those of benign lesions. All four false positive cases, as suggested by exponential ADC, were idiopathic granulomatous mastitis. There were four false negative
lesions taking exponential ADC cutoff of 0.4, which includes one case of pure mucinous carcinoma, one case of mixed mucinous carcinoma, and two cases of invasive intraductal carcinomas in comparison to ten false negative lesions suggested by ADC (which includes seven cases of invasive intraductal carcinomas, one case each of invasive metaplastic, pure and mixed mucinous carcinomas). Both pure mucinous carcinoma [Figure 6] and mixed mucinous carcinoma showed higher ADC values ($1.86 \times 10^{-3}$ mm$^2$/s and $1.53 \times 10^{-3}$ mm$^2$/s, respectively) and lower exponential ADC values (0.226 and 0.303, respectively), giving false negative results. These lesions reduced the specificity of DWI.

High ADC and lower exponential ADC values were observed in cases of both pure and mixed mucinous carcinomas, which may be due to low density of tumor cells and rich mucin content as compared to high cellularity of IDC. These results are in agreement with the the results of Jin et al.[21] and Woodhams et al.[22] in whose study the mucinous carcinoma showed very high ADC values. Regarding false positive case, idiopathic granulomatous mastitis [Figure 7] showed relatively low ADC values and high exponential ADC values. Bansal et al.[19] also reported false positive results in case of idiopathic granulomatous mastitis.

**Limitations of the study**

Our study has some limitations. First, lesions less than 1 cm were not included in the study as placement of ROI and interpretation of ADC and exponential ADC would have been difficult and erroneous due to partial volume effect.

Second, absence of in-situ and grade I breast carcinomas in the study which reflects the current presentation of breast carcinoma in a tertiary care centre of eastern India, where breast carcinomas are diagnosed at an advanced stage in a majority of cases due to lack of awareness among local women and standardized screening protocol. Cut-off values obtained in this study might not be generalizable to other DWI acquisition schemes because of disunified diffusion gradient factor $b$. A large cohort is required to validate the results. Finally, overlap still existed between ADC and exponential ADC map values between benign and malignant lesions. ADC and exponential ADC maP values may be unreliable for mucinous carcinoma and idiopathic granulomatous mastitis.

**Conclusion**

Exponential ADC can be used as a quantitative adjunct tool for characterizing breast lesions with comparable sensitivity and specificity as that of ADC, apart from being used as a visual aid to the radiologist and clinicians. However, DWI and its quantitative parameters ADC and exponential ADC have a limited role in evaluating idiopathic granulomatous mastitis and mucinous carcinomas. More studies are required to validate the role of exponential ADC in characterizing breast lesions.

**Financial support and sponsorship**

Nil.

**Conflicts of interest**

There are no conflicts of interest.
Figure 6 (A-G): 41 year old woman with pure mucinous carcinoma in left breast. Axial DWI (b 800s/mm²) shows tumor as high signal intensity in both DWI and ADC map images (A and B) and low signal intensity in corresponding exponential ADC image (C), consistent with no diffusion restriction. ADC and EXPONENTIAL ADC values were 0.00186 mm²/s and 0.226 respectively. Lesion shows mixed signal intensity on T2WI (D) and heterogenous enhancement on post contrast study (E). (F) (H&E 10x10) & (G) (H&E 40x10) showing clumps of malignant ductal cells floating in pools of extracellular mucin.

Figure 7 (A-F): 49 year women with idiopathic granulomatous mastitis of left breast. Axial DWI at b800s/mm² shows areas of hyperintensity within the mass (A) with corresponding areas of hypointensity in ADC image (B) and hyperintensity in EXPONENTIAL ADC image (C), consistent with diffusion restriction. ADC and EXPONENTIAL ADC values were 0.000632 mm²/s and 0.604 respectively. Lesion is hypointense on axial T2WI (D) & shows heterogenous enhancement in post contrast study (E) (H&E 40x10): Microphotograph shows presence of collection of epithelioid cells in fibrocollagenous stroma (F).
References


