Influence of Different Restoring Materials on Stress Distribution in Prosthesis on Implants: A Review of Finite Element Studies

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Abstract

The selection of material used on the occlusal surface of implant-supported protheses is important, as these materials can transmit destructive forces to the interface between the alveolar bone and the implant. Different prosthetic materials are suggested for implant-supported protheses. The choice of prosthetic material is a controversial issue, and there is a consensus that implant survival is not affected by the prosthetic material. Three-dimensional finite element studies are often used in dentistry to estimate the stress distribution that occurs in the implant system, peri-implant bone, and prosthetic components. To analyze the influence of the prosthetic restorative material on the stresses in bone tissue and peri-implant through a literature review of three-dimensional finite element studies. The search for articles was performed in the PubMed/Medline database up to November 2021. The selected articles were independently evaluated by two different reviewers. The information collected was author and year of publication, dimensions of implants used, the material used in the prosthetic crown, simulated force and direction, and conclusion and effect.

After searching, 14 studies were selected for full reading, and based on the inclusion and exclusion criteria, all could be included in this review. The articles were based on evidence-based laboratory medicine. After analyzing these articles, it was concluded that the prosthetic materials used on the occlusal surface do not interfere with the destruction of stresses to the bone and peri-implant tissue, both in single protheses and protocol-type protheses, when three-dimensional finite element method is used.

Keywords

- dental implant
- finite element analysis
- ceramics
- occlusal surface


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Introduction

Dental implants have improved the quality of life of millions of patients in recent decades and have shown a high predictability of success. The high success rates and long-term follow-up (over 20 years) of patients treated with osseointegrated dental implants have attracted the interest of clinicians and researchers worldwide. Occlusal loading of osseointegrated implants is a determining factor in the longevity of treatments with implants. The selection of material used on the occlusal surface of implant-supported prostheses is also important, as these materials can transmit damaging forces to the interface between the alveolar bone and the implant.

Different prosthetic materials are suggested for the fabrication of implant-supported prostheses. The choice of this material is controversial although there is a consensus that implant survival is not affected by the prosthetic material. Skalak et al stated the theory that loading an implant made of a hard occlusal material, either porcelain or metal, can result in high-intensity loading between the implant and the supporting bone. While a material with a low modulus of elasticity has stress-absorbing properties, it can prevent the surrounding bone from possible destruction linked to the magnitude of the load.

Three-dimensional finite element analyses (3D-FEA) are frequently used in dentistry to estimate the stress distribution that occurs in the implant system, peri-implant bone, and prosthetic components. 3D-FEA allows the simulation of a condition that would be impossible to achieve in a clinical study. Therefore, traditional finite elements have become a useful tool to study stress distribution in implant dentistry.

The purpose of this review of the literature on finite element studies is to investigate the influence of the prosthetic material on the stresses induced in bone tissue in implant-supported prostheses.

Methods

The search for articles of this review of the literature was performed in the PubMed/Medline database for articles published up to November 2021. The search strategy used was (finite element analysis) AND (occlusal device OR occlusal surface OR occlusal materials OR veneering materials) AND (implants OR dental implants). The inclusion criteria were studies using the 3D-FEA methodology that evaluated the stress distribution in bone tissue, among different prosthetic/restorative materials, published only in English. The exclusion criteria were studies that did not follow the 3D-FEA methodology. The selected articles were independently evaluated by two different reviewers. The information collected was author and year of publication, dimensions of implants used, the material used in the prosthetic crown, simulated force and direction, and conclusion and effect.

Articles of the in vitro study were selected following evidence-based laboratory medicine. These principles are (1) asking the question, (2) searching for evidence, (3) appraising the evidence, (4) applying the evidence, and (5) assessing the experience.

Results

During the search process, 314 references were found, of which 14 were selected after reading the title and abstract, to be analyzed for their full-text. After this step, all 14 articles were included for data collection. The search strategy is detailed in Fig. 1. The individual details of the studies included in this review can be seen in Table 1.

The selected studies were dated from 1996 to 2021. The simulated implants were of varying diameters, ranging from 3.8 mm to 5 mm. The length of the implants also varied, with the shortest length being 7 mm and the longest being 13 mm. Regarding the prosthetic materials, a variety of metal-ceramic prostheses can be seen, varying the material of the infrastructure and the veneering ceramic, in addition, prostheses in lithium disilicate and zirconia, acrylic resin, and composite resin. The simulated forces ranged from 30 to 1000 N, using either axial or oblique loads.

Twelve studies found no differences in force dissipation in bone tissue between different prosthetic materials. Only two studies found a positive relationship between the restorative material and bone tissue tension.

Discussion

Biomechanical considerations are recognized as being one of the most important factors for the long-term success of osseointegrated implants. Among the methods for evaluating implant biomechanics, 3D-FEA has been widely used for the quantitative assessment of bone stresses. This analysis identifies stresses and their dissipation at the prosthesis-
### Table 1 Characteristics of the studies included in this review

<table>
<thead>
<tr>
<th>Author</th>
<th>Implant information</th>
<th>Prosthetic crown</th>
<th>Simulated force</th>
<th>Outcome</th>
<th>Effect</th>
</tr>
</thead>
<tbody>
<tr>
<td>Yegin and Atala, 2020</td>
<td>Internal connection at the level 4.1 mm × 12 mm</td>
<td>Lower first molar 1. Monolithic LD 2. LD as a veneering ceramic 3. LD reinforced with monolithic zirconia 4. Reinforced LD as a veneering ceramic</td>
<td>300 N Axial</td>
<td>Von Mises stresses were relatively similar and concentrated in the coronal part of implants and abutments in all groups. The different restorative materials did not influence the stress distribution although monolithic crowns reduced the stress concentration on the implant and the bone.</td>
<td>Negative</td>
</tr>
<tr>
<td>Mendes Tribst et al, 2019</td>
<td>Internal hexagon 3.75 mm × 11 mm</td>
<td>Molar 1. Monolithic zirconia 2. Monolithic LD 3. Monolithic Hybrid Ceramics</td>
<td>300 N Oblique (30°)</td>
<td>There were no differences between zirconia, LD, and hybrid ceramic crowns in the distribution of forces in the bone. The use of the combination of a crown with a low modulus of elasticity and a mesostructure with a high modulus of elasticity on Ti-base demonstrated a better dissipation of forces.</td>
<td>Negative</td>
</tr>
<tr>
<td>Sotto-Maior et al, 2012</td>
<td>External hexagon 5 mm × 7 mm</td>
<td>Lower first molar 1. PFM (Gold IV infrastructure and feldspathic ceramic veneer) 2. All-ceramic (zirconia framework and feldspathic ceramic veneer)</td>
<td>200 N Axial Oblique (45°)</td>
<td>The dissipation of forces was not influenced by the prosthetic material, the occlusal force is the factor that has the greatest weight concerning the stresses generated in the implants, the second most important being the abutment.</td>
<td>Negative</td>
</tr>
<tr>
<td>Sevimay et al, 2005</td>
<td>4.1 mm × 10 mm</td>
<td>Lower second premolar 1. IPS Empress 2 2. In-Ceram 3. PFM with cobalt-chromium 4. PFM with gold-silver-palladium</td>
<td>300 N Axial</td>
<td>Different materials did not influence the distribution of forces in the bone and peri-implant bone tissue. However, in the abutment and crown structure, stress distributions and locations were affected by the stiffness of the material, because materials with the highest modulus of elasticity concentrated higher stress.</td>
<td>Negative</td>
</tr>
<tr>
<td>Sanninno et al, 2010</td>
<td>4.5 mm × 13 mm</td>
<td>1. Zirconia 2. Micro-hybrid composite</td>
<td>30 N 60 N 120 N 240 N 500 N 600 N 800 N Axial and oblique (45°)</td>
<td>In axial loading, the use of zirconia in the abutment and crown allows for less tension (~5–10%) than the other combinations of materials investigated, in the bone region around the implant neck. In oblique loads, the use of titanium abutment and a micro-hybrid crown composite allows for the transfer of occlusal loads more uniformly and with slightly lower peak von Mises stress values (7–11%) than in the other cases. However, this material choice, as well as the combination of zirconia abutment and micro-hybrid composite in the crown, produces the greatest stress gradients in the cement layer.</td>
<td>Positive</td>
</tr>
<tr>
<td>Author</td>
<td>Implant information</td>
<td>Prosthetic crown</td>
<td>Simulated force</td>
<td>Outcome</td>
<td>Effect</td>
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<tr>
<td>Juodzbalys et al, 2005</td>
<td>3.8 mm / C2</td>
<td>1. Vita VMK 68 Seer 2. GC GRADIA</td>
<td>143 N - 0° 500 N - 90° 1000 N - 120°</td>
<td>Lower first molar</td>
<td>Negative</td>
</tr>
<tr>
<td></td>
<td></td>
<td></td>
<td>76.5N Axial 534 N Oblique (30°)</td>
<td></td>
<td></td>
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<tr>
<td></td>
<td></td>
<td></td>
<td>200 N Axial 100 N Oblique (30°)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Gungor and Yilmaz, 2014</td>
<td>4 mm x 12 mm</td>
<td>1. LD 2. Zirconia</td>
<td>76.5 N Axial 534 N Oblique (30°)</td>
<td>Fixed partial prosthesis (central incisor, lateral incisor, and canine)</td>
<td>Negative</td>
</tr>
<tr>
<td>Mourya et al, 2021</td>
<td>4 mm x 12 mm</td>
<td>1. PFM 2. PEEK</td>
<td>1000 N Axial 500 N Oblique (30°)</td>
<td></td>
<td>Negative</td>
</tr>
<tr>
<td>Ercal et al, 2021</td>
<td>4 mm x 11.5 mm</td>
<td>1. Lower premolar 2. PFM</td>
<td>1000 N Axial 500 N Oblique (30°)</td>
<td></td>
<td>Positive</td>
</tr>
<tr>
<td>Papavasiliou et al, 1996</td>
<td>4 mm x 12 mm</td>
<td>1. Gold coated with acrylic resin 2. PFM</td>
<td>200 N Axial</td>
<td></td>
<td>Negative</td>
</tr>
<tr>
<td>Ferreira et al, 2021</td>
<td>4 mm x 10 mm</td>
<td>1. PFM 2. Acrylic resin 3. Porcelain</td>
<td>172 N Axial</td>
<td></td>
<td>Negative</td>
</tr>
<tr>
<td>Lemos et al, 2021</td>
<td>4 mm x 10 mm</td>
<td>1. PFM 2. Monolithic zirconia</td>
<td>200 N Axial 100 N Oblique</td>
<td></td>
<td>Negative</td>
</tr>
</tbody>
</table>

Abbreviations: LD, lithium disilicate; N, Newtons; PFM, porcelain fused to metal; PEEK, polyetheretherketone.
implant-bone interface, which can be difficult to assess by other biomechanical methods. After the review of included studies, it was found that most of the articles indicate that the prosthetic material does not influence the generation of tension and dissipation in the bone and peri-implant tissue. This can be justified due to the use of different prosthetic materials having less influence on the stresses in the supporting bone with 1% of the variance. According to Sotto-Maior et al, the dissipation of forces was not influenced by the prosthetic material although the occlusal force is the factor that has the highest weight about the stresses generated in the implants, abutment being the second. Despite not affecting bone tissue, occlusal materials show differences in stress distributions in the crown structure and abutment.

Sevimay et al evaluated prosthetic crowns made with IPS Empress 2, In-Ceram, PFM with a chromium-cobalt framework, PFM with a gold-silver-palladium framework, and states that the different prosthetic materials did not influence the distribution of forces in bone and peri-implant bone tissue. However, when evaluating the ceramic, IPS Empress 2 showed the highest stress concentration. When the stress distribution in the framework was evaluated, the stress values were different for each model. In-Ceram porcelain (173 MPa) and PFM crown with a cobalt-chromium framework (149 MPa) induced higher von Mises stress values than PFM crown with a gold-silver-palladium framework (108 MPa) and IPS Empress 2 (119 MPa). The reason for these differences may be related to the elastic modulus of the materials. In-Ceram and PFM crown with chromium-cobalt framework have a higher modulus of elasticity compared with IPS Empress 2 and PFM crown with a gold-silver-palladium framework. Sannino et al analyzed the stresses of the prosthesis-implant system and showed that the choice of material was crucial for the distribution of stresses in different components. It was noted that due to the large difference in the hardness between the materials of the system, the main stress gradient in the cement layer increased in the situation of zirconia abutment with micro-hybrid composite core and titanium abutment with a micro-hybrid composite core. For the situation of zirconia on abutment and core, and titanium abutment and zirconia core, the stress distribution in the cement layer was more homogeneous. Higher failure risks for the cement layer placed between the core and the abutments were found when a micro-hybrid composite core was used.

Gungor and Yilmaz reported that higher stress levels were observed in the models with zirconia (93.6 MPa) compared with models with lithium disilicate (76.3 MPa). One justification for this is that stresses in the framework materials increased with the decrease in the modulus of elasticity of the layering material. Higher differences between the modulus of elasticity of the framework and the veneer material transmit greater concentrations of stress in the framework. Yegin and Atala also agree that higher differences between the modulus of elasticity of the infrastructure and the veneer ceramics lead to a higher concentration of stress in the framework. Thus, the monolithic crowns showed a decrease in stress concentration, as the stresses were more concentrated on the ceramic surface due to the elastic modulus being the same throughout the prosthesis, which reduced the load transmission to the implant and the bone, consequently.

The study by Mourya et al reveals that the use of a material with a lower modulus of elasticity in the crown, such as PEEK crowns with a composite resin layer, implies greater stress on the abutment than a metal-ceramic crown. The PEEK group in the axial loading presents 514 MPa in the abutment, while the metal-fused porcelain crown has a tension of 123 Mpa. In the oblique loading, which is the most harmful to the implants, these values increase to 1347 MPa (PEEK) and 400 MPa (PFM). Due to this, the use of prosthetic materials with a low modulus of elasticity may be associated with failures in the abutment region, with the retaining screw being the most subject to failure. Alves Gomes et al observed that porcelain crowns absorbed less stress than composite resin crowns. The use of porcelain as a veneer material reduced the stress that was transmitted to the retaining screw. Composite resin has a low modulus of elasticity and is more deformable than porcelain. Thus, resin exhibits greater displacement and transfers stress directly to the retaining screw, different from the porcelain. Low abrasion resistance is a disadvantage of the composite resin. If the occlusal scheme and morphology cannot be maintained over time, undesirable lateral forces may increase.

When evaluating complete dentures fixed to implants, studies agreed that different occlusal materials did not influence the tension transmitted to the bone tissue. However, Ferreira et al shows that although the resin teeth had lower values of von Mises stress, the groups with porcelain teeth significantly decreased the stresses on the metallic frameworks. Although different occlusal materials do not influence the tension transmitted to the bone and peri-implant tissue, there is a tendency where materials with low elastic modulus transmit greater tensions to the infrastructure materials both in single prostheses and in protocol-type prostheses. In contrast to the 12 studies that did not show a positive relationship between the prosthetic material and the increase in stress in the bone tissue, two articles found a positive result, which can be explained by the different designs of the 3D-FEA studies, where the change in the implant geometry and bone density between studies may explain the discrepancies between the results. Finite element studies allow an approximation of the behavior of the material to the real situation.

Therefore, further investigations related to dynamic applications of forces and long-term clinical studies are needed to assist the dentist in choosing the appropriate prosthetic material in implant-supported restorations.

**Conclusion**

Evaluating the stress distribution by 3D-FEA, the prosthetic materials used on the occlusal surface did not interfere with
the distribution of stresses to the bone and peri-implant tissue, both in single prostheses and protocol-type prostheses.

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None.

Conflict of Interest
None declared.

References