Abstract

Purpose: To differentiate PCA segments and cortical branches by means of transcranial color-coded duplex sonography (TCCD) and to measure flow parameters at rest and during visual stimulation.

Materials and Methods: 60 healthy subjects with a good acoustic temporal bone window were examined. The main stem of the PCA (P1, P2 and P3) and 4 main cortical branches – the anterior temporal artery (ATA), the occipital temporal artery (OTA), the parietooccipital artery (POA) and the calcarine artery (CA) – were assessed using an axial transtemporal approach. Systolic and diastolic blood flow velocities (BFVs) were recorded at rest and during visual stimulation.

Results: Identification of the P1 segment of the PCA was successful in 97.5% (117/120) of cases. The P2 and P3 segments were visualized in all cases. The 4 main cortical branches could be identified to varying degrees: ATA in 88%, OTA in 96%, POA in 69% and CA in 62%. There was an evoked flow response in the P2 main stem and in all cortical branches. The most pronounced increase in diastolic/systolic BFV after visual stimulation test was seen in the CA (42%/35%), followed by P2 (30%/24%), the POA (27%/27%), the OTA (16%/13%) and the ATA (9%/8%).

Conclusion: Insonation through the temporal bone window with TCCD confidently allows the assessment of the P1 to P3 segments of the PCA as well as the 2 proximal branches, the ATA and the OTA. An ultrasound-based classification of PCA anatomy and its cortical branches may be used as a noninvasive method for the evaluation of posterior circulation pathology.
firm branch coursing in a posterolateral direction, supplying the inferior temporal and occipital surfaces and the lingual gyrus. The POA occurs as a single terminal branch, in about half of the cases arising from P3 as part of a terminal bifurcation with the CA. In 40% of cases it branches off the distal P2 and in 10% even from the proximal P2 [5]. From its medial origin the POA rises upward and laterally to the parietooccipital fissure and during its course often crosses the proximal calcarine fissure. The CA is the second terminal PCA branch. In about half of cases it arises from P3 but may depart from the distal P2 in 42% of cases. In 10% it may also branch off the POA [5]. Its irrigation area includes, but is not limited to, the visual cortex.

MRA and CTA techniques also allow good visualization of the major PCA branches, but no detailed assessment has been reported up to now [8, 9], and to our knowledge, no previous studies on flow rates measured with TCCD have been previously published. Early sonographic PCA assessments using transcerebral Doppler (TCD) divided the PCA into a P1 and P2 segment, based on the detected flow direction. A flow direction towards the transducer was defined as the P1 segment, and a flow away from the transducer as the P2 segment [10]. However, this nomenclature does not correspond to real anatomy. TCCD allows a more precise anatomical correlation and PCA assessment in relation to its junction with the PCoA. Using TCCD, the proximal P2 shows – identical to P1 – a flow direction towards the transducer and the distal P2 and P3 and P4 show a flow away from the transducer [11]. Based on anatomical data, we analyzed the main PCA segments as well as the PCA branches ATA, OTA, POA and CA, the latter of which have not yet been described and classified with TCCD. In addition, blood flow in the P2 segment as well as in the 4 cortical branches was analyzed during a visual stimulation test to prove the hypothesis that the magnitude of responses relate to each vessel’s participation in feeding the striatal and peristriatal visual cortex.

Materials and Methods

Healthy subjects with a sufficient acoustic temporal bone window, i.e., the M1 segment of the middle cerebral artery (MCA) and the P1 and P2 segment of the PCA were easily visualized on both sides, were recruited at the neurological center of the Segeberger Kliniken in Germany. Subjects with an insufficient acoustic temporal bone window were excluded. Informed written consent was obtained from all subjects. The study was approved...
formed using a Power Vision 6000 SSA-370 A ultrasound system. All vessels were examined using an axial insonation plane through the temporal bone window, which is most easily achieved by placing the probe directly preauricularly and superior to the zygomatic arch. In the mesencephalic plane, the P1 and the proximal P2 were visualized red-colored with a flow towards the transducer. The junction between P1 and P2 was defined by the concomitant visualization of the distal ICA if no PCoA was visible. The origin of the ATA was defined as a red-colored vessel at the junction between the proximal and distal P2 with a flow towards the probe. The origin of the OTA was defined as a comma-shaped, red-colored vessel at the distal P2. Reflecting the slightly upward vessel course, the distal P2 was defined by its blue-colored visualization with a flow away from the probe mainly in a midbrain–thalamic insonation plane. P3 was defined as the main course of the PCA within the quadrigeminal cistern. A bifurcation in the quadrigeminal cistern or more distal in the thalamic plane was defined as the origin of the POA and CA, both vessels representing P4. A vessel course upward and lateral into the parietooccipital fissure (between the thalamic and the cella media plane) was allocated to the POA. A midbrain-plane vessel course near to the interhemispheric space was allocated to the CA. In cases of doubt regarding the differentiation between the POA and CA, the vessel with the stronger response to the visual stimulation test was defined as the CA.

The systolic and diastolic blood flow velocity (BFV) in the PCA main stem and the cortical branches was measured at rest and during a visual stimulation test. Since the depicted vessels were curved or their length was usually short (<1 cm), all flow velocity measurements were performed without angle correction. Subjects were examined on both sides. Baseline systolic and diastolic BFVs were measured with the subject’s eyes closed. Visual activation was achieved by eye opening and looking at a checker-chart on the ceiling for 20 s. BFVs were measured at the end of the 20 s and the increase of flow was calculated as the percent increase above baseline levels for all studied vessels. Statistical analysis of the difference in average BFV increase between branches was performed using the Kruskal-Wallis test (non-parametric ANOVA) and multiple comparisons between the 5 groups were performed using Dunn’s post-test.

### Table 1
PCA main stem detection rates and flow velocities.

<table>
<thead>
<tr>
<th>Detection rate (%)</th>
<th>V diast (cm/s)</th>
<th>V syst (cm/s)</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>P1</strong> 97.5</td>
<td>28.1 ± 8.5 (11–52)</td>
<td>59.8 ± 14.3 (27–103)</td>
</tr>
<tr>
<td><strong>P2</strong> 100</td>
<td>27 ± 6 (16–43)</td>
<td>58 ± 11 (39–104)</td>
</tr>
<tr>
<td><strong>P3</strong> 100</td>
<td>29.9 ± 7.9 (18–58)</td>
<td>62.6 ± 12.0 (30–94)</td>
</tr>
</tbody>
</table>

Mean ± standard deviation, range ( ), flow velocities without angle correction.

### Table 2
PCA cortical branches: detection rates, flow velocities and response to checker-chart visual stimulation.

<table>
<thead>
<tr>
<th>Detection rate (%)</th>
<th>V diast at rest (cm/s)</th>
<th>V diast stimulation (cm/s)</th>
<th>Change V diast (%)</th>
<th>V syst at rest (cm/s)</th>
<th>V syst stimulation (cm/s)</th>
<th>Change V syst (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>ATA</strong> 88</td>
<td>12 ± 4 (5–2)</td>
<td>13 ± 5 (7–30)</td>
<td>8.5</td>
<td>26 ± 9 (12–56)</td>
<td>28 ± 11 (13–63)</td>
<td>8.2</td>
</tr>
<tr>
<td><strong>OTA</strong> 96</td>
<td>16 ± 5 (8–27)</td>
<td>19 ± 9 (9–35)</td>
<td>16</td>
<td>34 ± 9 (18–57)</td>
<td>38 ± 12 (19–70)</td>
<td>12.6</td>
</tr>
<tr>
<td><strong>POA</strong> 69</td>
<td>21 ± 8 (9–62)</td>
<td>26 ± 10 (10–71)</td>
<td>27.4</td>
<td>40 ± 14 (19–100)</td>
<td>51 ± 18 (23–124)</td>
<td>27.1</td>
</tr>
<tr>
<td><strong>CA</strong> 62</td>
<td>16 ± 6 (5–31)</td>
<td>22 ± 8 (7–47)</td>
<td>41.6</td>
<td>33 ± 10 (14–62)</td>
<td>43 ± 13 (19–83)</td>
<td>34.7</td>
</tr>
<tr>
<td><strong>P2</strong> 100</td>
<td>27 ± 6 (16–43)</td>
<td>34 ± 8 (20–52)</td>
<td>29.5</td>
<td>58 ± 11 (39–104)</td>
<td>72 ± 13 (48–117)</td>
<td>23.9</td>
</tr>
</tbody>
</table>

Mean ± standard deviation, range ( ), flow velocities without angle correction.

### Results

60 healthy subjects, aged 18–62 years (39±10.9), were included in the study. P1 was successfully identified in 97.5% (117/120) of the cases. P2 and P3 were visualized in all cases. BFVs were almost identical with slightly higher values in P2 and P3 compared with P1 (Table 1).

Following the defined criteria, the 4 main cortical PCA branches were identified to varying degrees: ATA in 88% of cases, OTA in 96% of cases, POA and CA in 69% and 62% of cases, respectively. The highest BFVs were measured in the POA, followed by the CA and the OTA with similar values. The ATA showed the lowest BFVs (Table 2).

Visual stimulation led to a BFV increase in P2 and all 4 cortical PCA branches. The most pronounced increase in diastolic/systolic BFV was found in the CA (42%/35%), followed by P2 (30%/24%), the POA (27%/27%), the OTA (16%/13%) and the ATA (9%/8%) (Table 2). Non-parametric ANOVA yielded a significant difference for diastolic and systolic flow increases (KW=123.06 and 106.53, p<0.0001). Multiple comparisons (systolic and diastolic BFV rise) showed a significant difference between groups (p<0.01) except for the comparison of PCA vs. POA and ATA vs. OTA.
**Discussion**

This study shows that the main segments of the PCA as well as the most relevant cortical branches can be identified by TCCD and differentiated according to real anatomical conditions. In addition, a separate analysis of flow responses to visual stimulation in selected cortical branches of the PCA has not been published previously.

In our study, the segments P1 to P3 were visualized in nearly all of our cases. Similar high detection rates of 72–100 % have been reported for P1 and P2 [12–15]. Data for the cortical branches, however, were missing. The 2 proximal branches, the ATA and OTA, can be reliably identified with non-contrast-enhanced TCCD. The detection rates of 82 % (ATA) and 96 % (OTA) correspond with the anatomical data of Zeal who reported rates of 84 % and 96 %, respectively [5]. In contrast, the detection rates differ markedly in regard to the POA and CA with detection rates of 69 % and 62 % but an anatomical presence in 96 % and 100 %, respectively [5]. The main reason for this may be the restriction of insonation quality through the temporal bone for the visualization of more dorsally located vessels.

Regarding flow rate response to visual stimulation, our reported BFVs in P1 and P2 correspond to the data from the literature [12–14]. The highest cortical branch BFVs with closed eyes were found in the POA, followed by the OTA, CA and ATA. The vessel diameter is correlated to the significance of the artery and absolute BFV values correspond to the amount of perfused brain parenchyma by the selected artery. The perfusion area of the POA includes large parietal and occipital areas and that of the OTA temporal and occipital areas whereas the CA is more restricted to anterior parts of the temporal lobe and the hippocampus. The wide inter-individual range in BFV in selected branches indicates the high variability in the perfusion area. This has been shown in anatomical studies for the OTA and CA [16]. Our findings are in good accordance with the anatomical literature. Diameter measurements of the POA, OTA, CA and ATA were reported to be 1.6 mm, 1.6 mm, 1.4 mm and 1.3 mm, respectively [5]. Similar data of 1.5 mm, 1.6 mm, 1.3 mm and 1.2 mm were reported recently.

Like functional magnetic resonance imaging (fMRI) and positron emission tomography (PET), ultrasound allows the assessment of changes in local neuronal activity by measuring changes in blood flow velocities in a selected vessel segment, which corresponds to changes in regional blood flow (rCBF). In contrast to MRI and PET, ultrasound methods have a high temporal resolution allowing instant assessment of regional CBF changes. The major disadvantage of functional ultrasound, however, is the limited spatial resolution. Despite this, a large number of studies using TCD focusing on sensory, motor and cognitive functions, especially concerning language lateralization in man have been published in recent years [17, 18]. An evoked flow response of PCA main stem flow to visual stimuli has been demonstrated using TCD shortly after its introduction in clinical medicine with a mean BFV increase of about 20 % in healthy subjects [19–22]. PCA visual evoked flow has been used to separate PCA signals from vessels of the anterior circulation and from the superior cerebellar artery (SCA) [23] and to distinguish patients in a vegetative state [24].

However, data on flow responses in select cortical branches has not previously been reported. Our results show that the major evoked increase in diastolic BFVs after visual stimulation was as expected in the CA with 41.6 % followed by the POA and OTA with 27.4 % and 16.2 %, respectively. The weakest effect was observed in the ATA with an increase of 8.5 % only. The obvious response in the POA and less in the OTA may be explained by their contribution to the perfusion of the striatal and peristriatal cortex in 20–35 % and 3–22.5 % of cases, respectively. The P2 segment showed an increase of diastolic BFV of 29.5 %, which corresponds to discussed data from the literature [25–26].

Our observations may be doubly useful. First, the new TCCD vessel nomenclature allows a more exact anatomical description of PCA vessel anatomy and pathology. Instead of mere detection of main stem PCA pathology [27, 28], the newly described PCA segments may facilitate the recognition of vessel stenoses in more distal parts and in selected branches. It may also facilitate a more precise definition of main stem occlusions and a more elaborate description of collateral leptomeningeal PCA flow in MCA occlusion [25, 26].

Second, the ability to examine select cortical branches may open new possibilities in functional Doppler of the visual system. One major obstacle of TCCD is that it allows only hand-held examination of the vessels, limiting the measurement of BFV changes during the visual task. Here, either newly developed TCCD probe holders, or information transfer (depth, probe position, waveform, BFV, and flow direction) from TCCD to TCD, might be a solution.

Limitations of our study have to be mentioned. One is the subjects' relatively young age. A lower frequency of successful visualization in older subjects is expected due to a diminished temporal acoustic window. The use of echo-contrast agents can ameliorate the sensitivity of TCCD markedly [29]. However, the use of a contrast agent may require that different reference values are used [30]. Also, variations of PCA cortical branches have to be considered, e.g., a common temporal branch which bifurcates or trifurcates into several smaller branches, a middle temporal artery between the OTA and ATA, or a small hippocampal artery present as the first cortical branch of the PCA [5], leading to confusion with the ATA. Also a prominent posterior choroid or posterior pericallosal artery may arise from the P2 and P3 segments [23]. Finally, the main stem of the PCA may be confused with the SCA, which runs parallel and close together with the PCA at their origins from the basilar artery [23].

**Conclusion**

Non-contrast-enhanced TCCD insonation through the temporal bone window allows visualization not only of the PCA main stem from the P1 to the P3 segments but also the cortical PCA branches, with the proximal ATA and OTA more readily visualized than the peripherally located POA and CA. The above nomenclature allows more accurate assessment of vascular disease location. Evoked flow velocity responses to a visual stimulus can be analyzed in PCA branches. Different reaction patterns can be used to distinguish branches, e.g., the POA from the CA, and open the door for new functional testing in cognitive and visual disorders.

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