Cardiac MRI: T2-Mapping Versus T2-Weighted Dark-Blood TSE Imaging for Myocardial Edema Visualization in Acute Myocardial Infarction

Kardiales MRT: T2-Mapping versus T2-gewichtete TSE-Bildgebung für die Visualisierung eines Myokardödems beim akuten Myokardinfarkt

Authors
K. Naßenstein1, F. Nensa1, T. Schlosser1, O. Bruder2, L. Umutlu1, T. Lauenstein1, S. Maderwald3, M. E. Ladd3

Affiliations
1 Dep. of Diagnostic and Interventional Radiology and Neuroradiology, University Hospital Essen
2 Department of Cardiology and Angiology, Contilla Heart and Vascular Center, Elisabeth Hospital Essen
3 Erwin L. Hahn Institute for Magnetic Resonance Imaging, University Duisburg-Essen

Correspondence
Dr. Kai Naßenstein
Institut für Diagnostische und Interventionelle Radiologie und Neuroradiologie, Universitätsklinikum Essen
Hufelandstraße 55
45122 Essen
Germany
Tel.: ++ 49/02 01/7 23 23 11
Fax: ++ 49/02 01/7 23 15 48
Kai.Nassenstein@uni-due.de

Abstract

Purpose: To assess the diagnostic accuracy of T2 mapping for the detection of myocardial edema in acute myocardial infarction (AMI), and to compare this diagnostic accuracy with that of the current standard for myocardial edema imaging, which is T2w dark-blood TSE imaging.

Materials and Methods: 29 patients with AMI were examined at 1.5 T. For the visualization of myocardial edema, T2 maps, calculated from three T2w SSFP images, and T2w dark-blood TSE images were acquired in standard short- and long-axis views. Cine SSFP images were acquired for the analysis of left ventricular (LV) function and late gadolinium enhancement images (LGE) for the visualization of myocardial necrosis. The T2 maps as well as the T2w dark-blood TSE images were evaluated twice independently from the cine SSFP and LGE images. The presence or absence of myocardial edema was rated visually for each LV segment. As the standard of reference, the infarct zone was defined based on the cine SSFP and LGE images.

Results: In this segment-based analysis, T2 mapping showed a sensitivity of 82 % and a specificity of 94 % for the detection of edema in the infarct zone. T2w dark-blood TSE imaging revealed a sensitivity of 50 % and a specificity of 98 %. T2 mapping showed a higher intra-rater agreement compared to T2w dark-blood TSE imaging (κ: 0.87 vs. 0.76).

Conclusions: T2 mapping allows for the visualization of myocardial edema in AMI with a higher sensitivity and specificity, and features better diagnostic accuracy in terms of a higher sensitivity compared to T2w dark-blood TSE imaging.

Citation Format:
Introduction

Within the last decade, cardiac magnetic resonance imaging (CMR) has become an important diagnostic tool for the assessment of acute myocardial infarction (AMI) because it allows the visualization and quantification of myocardial necrosis and microvascular obstruction as well as the analysis and quantification of global and regional left ventricular (LV) function within a single examination [1–4]. Beyond the assessment of these important prognostic parameters, CMR allows the visualization of myocardial edema by the acquisition of T2-weighted images [5]. The detection of myocardial edema in the setting of myocardial ischemia is important since it permits the differentiation between areas of acute and chronic myocardial infarction [6], and, moreover, the determination of the area at risk of infarction [7].

Currently, T2-weighted turbo-spin-echo (TSE) sequences with dark-blood preparation are the standard for myocardial edema imaging in the clinical routine [8, 9]. Unfortunately, T2-weighted dark-blood TSE sequences are prone to image artifacts such as signal intensity variations caused by the use of phased-array coils, bright rim artifacts next to the endocardium caused by insufficient suppression of the signal from slow flowing blood, or posterior wall signal loss caused by through-plane motion of the dark-blood prepared slice out of the imaging slice in the case of improper timing [10–12]. Consequently, Kellman et al. showed that T2-weighted dark-blood TSE imaging was either non-diagnostic or incorrect in 29% of patients with AMI [13].

Recently, a quantitative T2 mapping technique that overcomes these limitations has been introduced for the evaluation of myocardial edema [14]. In short, this technique is based on the acquisition of three T2-prepared steady state free precession (SSFP) images, each acquired with a different T2 preparation time. Since image acquisition is done in the transient mode of single-shot SSFP immediately after T2 preparation, the signal in each image is dominated by the T2 preparation and, therefore, represents a different echo time along the T2 decay curve, thus enabling the calculation of the T2 relaxation times of each image pixel [14].

In a first clinical study, Verhaert et al. recorded the myocardial T2 values prospectively in 16 myocardial segments in 27 patients admitted with AMI and demonstrated that the average T2 values are higher in the infarct zone compared to remote myocardium [15]. Since in this study the infarct zone had been defined independently from the T2 maps based on the analysis of cine images and late gadolinium enhancement (LGE) images, and the T2 values of the infarct zone and remote myocardium had been calculated, thereafter, based on these predefined areas, the study of Verhaert et al. does not allow a statement concerning the diagnostic accuracy of T2 mapping independent of other sequences (e.g. cine images, LGE) [15]. However, beyond the quantification of T2 values in predefined areas, an essential requirement for edema imaging is that it enables reliable determination between edematous and non-edematous myocardium independent of other sequences (e.g. for diagnosis of acute myocarditis [9]).

Therefore, our study aimed to analyze the accuracy of T2 mapping for visual myocardial edema detection on a segmental basis in patients with AMI in comparison to the current standard for myocardial edema imaging, which is T2-weighted TSE imaging with dark blood preparation [8, 9].

Subjects and Methods

The study was approved by the local ethics committee, and written informed consent was obtained from all patients prior to CMR. Patients with a first AMI as defined by established diagnostic criteria [16] were consecutively enrolled. Both ST-segment elevation myocardial infarction (STEMI) and non-ST-segment elevation myocardial infarction (NSTEMI) were considered eligible. Patients with impaired renal function defined as a glomerular filtration rate (GFR) < 60 ml/min/1.73 m² were excluded from the study as well as patients with a known history of chronic myocardial infarction or general contraindications for magnetic resonance imaging (MRI).

During a period of 3 months, 29 consecutive patients (22 men, 7 women, mean age 59 ± 11 years) with a first AMI, who were willing to participate in the present study, were enrolled. 7 further patients (5 men, 2 women, mean age 63 ± 9 years), who were considered to be eligible for the present study, refused study participation. The baseline characteristics of the enrolled study population are given in Table 1 in detail.

Image acquisition

MR examinations were performed on a 1.5 Tesla MR scanner (Magnetom Avanto, Siemens Healthcare, Erlangen, Germany) equipped with high-performance gradients (SQ-Engine: maximum amplitude 45 mT/m, slew rate 200 mT/m/ms). For image acquisition, IQR interquartile range.

Table 1 Baseline characteristics of the study population (n = 29).

<table>
<thead>
<tr>
<th>cardiovascular risk factors</th>
<th></th>
<th></th>
</tr>
</thead>
<tbody>
<tr>
<td>hypertension</td>
<td>23 (79%)</td>
<td></td>
</tr>
<tr>
<td>hyperlipidemia</td>
<td>13 (45%)</td>
<td></td>
</tr>
<tr>
<td>hypercholesterolemia</td>
<td>6 (21%)</td>
<td></td>
</tr>
<tr>
<td>smoking history: current/former/never</td>
<td>12 (41%)/5 (17%)/12 (41%)</td>
<td></td>
</tr>
<tr>
<td>diabetes</td>
<td>4 (14%)</td>
<td></td>
</tr>
<tr>
<td>obesity</td>
<td>7 (24%)</td>
<td></td>
</tr>
<tr>
<td>previous myocardial infarction</td>
<td>0 (0%)</td>
<td></td>
</tr>
<tr>
<td>previous CABG</td>
<td>0 (0%)</td>
<td></td>
</tr>
<tr>
<td>previous PCI</td>
<td>0 (0%)</td>
<td></td>
</tr>
<tr>
<td>STEMI/NSTEMI</td>
<td>26 (90%)/3 (10%)</td>
<td></td>
</tr>
</tbody>
</table>

<table>
<thead>
<tr>
<th>laboratory diagnostics</th>
<th></th>
<th></th>
</tr>
</thead>
<tbody>
<tr>
<td>peak troponin T</td>
<td>median: 2.0; IQR: 2.89</td>
<td></td>
</tr>
<tr>
<td>creatine kinase (CK)</td>
<td>median: 971.0; IQR: 1650.75</td>
<td></td>
</tr>
<tr>
<td>creatine kinase MB (CK-MB)</td>
<td>median: 116.0; IQR: 174.25</td>
<td></td>
</tr>
<tr>
<td>culprit coronary artery</td>
<td></td>
<td></td>
</tr>
<tr>
<td>left anterior descending</td>
<td>15 (52%)</td>
<td></td>
</tr>
<tr>
<td>circumflex artery</td>
<td>5 (17%)</td>
<td></td>
</tr>
<tr>
<td>right coronary artery</td>
<td>9 (31%)</td>
<td></td>
</tr>
<tr>
<td>revascularization</td>
<td></td>
<td></td>
</tr>
<tr>
<td>PCI</td>
<td>28 (97%)</td>
<td></td>
</tr>
<tr>
<td>CABG</td>
<td>0 (0%)</td>
<td></td>
</tr>
<tr>
<td>none</td>
<td>1 (3%)</td>
<td></td>
</tr>
<tr>
<td>time between onset of symptoms and revascularization</td>
<td>median: 5.0 hours; IQR: 5.9 hours; range 1.0–149 hours</td>
<td></td>
</tr>
<tr>
<td>time between onset of symptoms and CMR</td>
<td>4.1 ± 2.8 days; range 1–10 days</td>
<td></td>
</tr>
</tbody>
</table>

Abbreviations: STEMI = ST-segment elevation myocardial infarction, NSTEMI = non-ST-segment elevation myocardial infarction, CABG = coronary artery bypass grafting, PCI = percutaneous coronary intervention, CMR = cardiac magnetic resonance imaging, IQR interquartile range.
acquisition, 6 elements of the spine matrix coil and all 6 elements of a phased-array torso coil (Tim Body Matrix Coil, Siemens Healthcare, Erlangen, Germany) were used.

A T2-weighted double inversion recovery (DIR) dark-blood prepared ECG-triggered, GRAPPA (GeneRalized Autocalibrating Partially Parallel Acquisition) accelerated, turbo-spin-echo (T2w DIR-TSE) sequence (echo time (TE) 74 ms, repetition time (TR) 2 × RR, angle of excitation (EA) 180°, echo train length 17, bandwidth 235 Hz/pixel, field of view (FOV) 244 × 300 mm² to 325 × 400 mm² depending on the anatomy of the individual patient, matrix 156 × 256, slice thickness 6 mm, acceleration factor 2) was acquired in standard short and long-axis orientation to visualize myocardial edema. To compensate coil sensitivity variations, the standard manufacturer’s coil sensitivity normalization (prescan normalization filter) was used.

For T2 mapping, three differently T2-prepared, GRAPPA accelerated, steady state free precession (SSFP) images (TR 3 × RR, FA 70°, echo spacing 2.5 ms, T2-preparation times (T2.p.) 0 ms/24 ms/55 ms, FOV 244 × 300 mm² to 325 × 400 mm² depending on the anatomy of the individual patient, matrix 104 × 160, bandwidth 947 Hz/pixel, slice thickness 6 mm, acceleration factor 2) were acquired in single-shot mode within one breath-hold per slice position. Although the sequence used ensures that all three images are acquired at the same point in the cardiac cycle, a non-rigid motion correction algorithm was used to adjust for moderate in-plane misregistration between the three images that may be caused by differences in cardiac cycle length or by a slight diaphragm position drift. From the three motion-corrected images, the T2 maps were automatically generated based on a linear 2-parameter model after logarithmic transformation, as previously described [14]. T2 maps were acquired in standard short and long-axis orientation similar to the T2w DIR-TSE images. A retrospectively ECG-gated, GRAPPA accelerated, SSFP sequence (TR 2.6 ms, TE 1.1 ms, EA 60°, FOV 244 × 300 mm² to 325 × 400 mm² depending on the anatomy of the individual patient, matrix 156 × 192, acquisition of 15 k-space lines per segment resulting in a temporal resolution of 39.5 ms, 25 calculated phases, bandwidth 930 Hz/pixel, slice thickness 6 mm, acceleration factor 2) was acquired in standard short and long-axis orientation for global and regional LV function analysis.

Inversion recovery (IR) spoiled-gradient-echo (GE) images (TR 8 ms, TE 4 ms, FA 30°, FOV 244 × 300 mm² to 325 × 400 mm² depending on the anatomy of the individual patient, matrix 172 × 256, slice thickness 6 mm, bandwidth 140 Hz/pixel) were acquired 10 – 15 minutes after intravenous injection of 0.2 mmol per kg body weight Gd-DTPA (Magnevist, Bayer Schering Pharma AG, Berlin, Germany) in standard short and long-axis views to visualize myocardial necrosis [17]. For each scan the optimal inversion time (TI) to null the signal of normal myocardium was determined by using an SSFP sequence with incrementally increasing inversion times (TE 1.2 ms, TR 2.4 ms, EA 50°, FOV 244 × 300 mm² to 325 × 400 mm² depending on the anatomy of the individual patient, matrix 78 x 192, slice thickness 8 mm, bandwidth 965 Hz/pixel, increasing inversion times (TI) in steps of 27.5 ms).

**Image analysis**

The T2w DIR-TSE datasets as well as the T2 maps were evaluated twice by one experienced observer (who had previously evaluated >5000 CMR) in randomized order without access to the other acquired sequences. A minimum time interval of 14 days was maintained between the two evaluations to avoid a systema-

tic bias. For semi-quantitative assessment of the extent of myocardial edema, an approach was used that had been described previously [18]. Based on the American Heart Association (AHA) segmental model of the left ventricle, the extent of edema was visually assessed for each LV segment, with the exception of segment 17 (apex), based on a 5-point scale: 0: no edema; 1: 1 - 25 % edematous myocardium; 2: 26 % to 50 % edematous myocardium; 3: 51 - 75 % edematous myocardium; 4: 76 % to 100 % edematous myocardium) for the T2 maps and T2w DIR-TSE datasets, and the segmental edema scores were summed to yield aggregate edema scores for each patient (possible range of the aggregate score: 0 (no edema visible in the entire LV myocardium) to 64 (edema of the entire LV myocardium). The image quality of T2w DIR-TSE images as well as of the T2 maps was visually analyzed based on a binary assessment (presence vs. absence of image artifacts that hamper the diagnostic value), and the number of segments with non-diagnostic image quality was assessed for both edema imaging approaches.

A second experienced observer (who had previously evaluated >4000 CMR), blinded to the edema imaging results, reviewed the cine and late gadolinium enhancement (LGE) images. Regional wall motion was visually evaluated and characterized as normal, hypokinetic, akinetic or dyskinetic for all cardiac segments. The extent of LGE within each myocardial segment was rated analog to the segmental assessment of myocardial edema, and similarly the segmental LGE scores were summed to yield an aggregate LGE score for each patient. As the standard of reference, the infarct zone was defined based on the cine and LGE images as well as on pertinent clinical information including coronary angiograms using the AHA 17-segment model of the left ventricle, whereby segment 17 (LV apex) was excluded from analysis. A segment of the LV was considered to be affected by acute ischemia if it belonged to the perfusion territory of the culprit coronary artery and showed an LGE in an ischemic pattern and/or a wall motion abnormality. Calculations of LV volumes and mass were performed based on the short-axis scans using ARGUS™ software (Siemens Healthcare, Erlangen, Germany) with semiautomated contour detection. Manual correction of the automatically rendered contours was performed in all cases. Papillary muscles and myocardial trabeculations were included into the ventricular cavity. End-diastole was defined visually as the phase of the cardiac cycle with the largest LV cavity at mid-ventricle, and end-systole as the phase with the smallest LV cavity. At the base of the heart, slices were considered to be in the left ventricle if at least 270° of the blood was surrounded by myocardium. The apical slice was defined as the last slice showing intra-cavity blood pool.

**Statistical analysis**

Statistical analysis was performed using MedCalc Version 11.4.2.0 (MedCalc Software, Mariakerke, Belgium). Continuous data with normal distribution are given as mean ± standard deviation, non-normally distributed data as median and inter-quartile range. Categorical data are expressed as frequency or percentage. The sensitivity, specificity, positive predictive values as well as negative predictive values were calculated for T2 mapping as well as for T2w DIR-TSE imaging. For statistical analysis, a two-tailed t-test for paired samples was used, or a Wilcoxon test in the case of non-normally distributed data. Cohen’s kappa coefficients were calculated for statistical analysis of the intra-rater reliability.
Results

Standard of reference: Definition of the infarct zone
Wall motion analysis revealed hypokinesia in 92, akinesia in 28, and dyskinesia in 3 LV segments resulting in a total of 123 LV segments with regional wall motion abnormalities. Assessment of LV volumes and global LV function revealed an end-diastolic volume of 133.6 ± 47.1 ml, an end-systolic volume of 64.6 ± 31.7 ml, a stroke volume of 69.0 ± 22.4 ml, and an ejection fraction of 53.0 ± 10.5 %. In 132 LV segments, myocardial necrosis was observed by LGE imaging, and a mean LGE score of 15.3 ± 7.0 (range 2 to 32) was observed. From the analysis of the cine and LGE images and the coronary angiograms, 139 LV segments were rated as affected and 325 as non-affected by AMI.

T2 mapping
T2 mapping revealed myocardial edema within the infarct zone in all patients (100 %) during the first blinded evaluation of the T2 maps and in 28 patients (96.6 %) during the second image analysis. Combining both blinded evaluations resulted in a sensitivity of 82.0 %, a specificity of 94.0 %, a positive predictive value of 85.4 %, and a negative predictive value of 92.4 % for the segment-based detection of myocardial edema within the infarct zone. Detailed results of the blinded reading are given in Table 2. Statistical analyses showed a very good intra-rater agreement concerning the segmental rating of myocardial segments as edematous or non-edematous (κ = 0.865; 95 % confidence interval 0.815 to 0.915). Both blinded evaluations resulted in a mean edema score of 17.8 ± 8.5. Statistical analysis showed no significant differences between the T2 map edema scores and the observed LGE score (17.7 ± 8.0 vs. 15.3 ± 7.0, p = 0.091; 17.8 ± 9.1 vs. 15.3 ± 7.0, p = 0.134 for the first and second evaluations, respectively). Image artifacts were observed in 3 of 369 (0.8 %) acquired T2 maps. However, all LV segments were rated as evaluable.

Table 2 Results of the blinded reading of the T2 mapping and T2w DIR-TSE datasets.

<table>
<thead>
<tr>
<th>T2 mapping</th>
<th>T2w DIR-TSE</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>1st blinded reading</td>
</tr>
<tr>
<td>LV segments rated as</td>
<td></td>
</tr>
<tr>
<td>edematous</td>
<td>131</td>
</tr>
<tr>
<td>non-edematous</td>
<td>333</td>
</tr>
<tr>
<td>edema score</td>
<td>17.7 ± 8.0</td>
</tr>
<tr>
<td>true positive</td>
<td>118</td>
</tr>
<tr>
<td>true negative</td>
<td>309</td>
</tr>
<tr>
<td>false positive</td>
<td>16</td>
</tr>
<tr>
<td>false negative</td>
<td>21</td>
</tr>
<tr>
<td>sensitivity</td>
<td>84.9 %</td>
</tr>
<tr>
<td>specificity</td>
<td>95.1 %</td>
</tr>
<tr>
<td>positive predictive value</td>
<td>88.1 %</td>
</tr>
<tr>
<td>negative predictive value</td>
<td>93.6 %</td>
</tr>
</tbody>
</table>

T2w DIR-TSE edema imaging
Overall, T2w DIR-TSE imaging revealed myocardial edema within the infarct zone in 24 patients (82.7 %) during the first blinded evaluation and in 21 patients (72.4 %) during the second image analysis. Combining both blinded evaluations resulted in a sensitivity of 50.4 %, a specificity of 98.0 %, a positive predictive value of 91.5 %, and a negative predictive value of 82.2 % for the segment-based detection of myocardial edema within the infarct zone. Detailed results of the blinded reading are given in Table 2. Statistical analysis revealed a good intra-rater agreement concerning the segmental rating of myocardial segments as edematous or non-edematous (κ = 0.76; 95 % confidence interval 0.68 to 0.84). Combining both blinded evaluations resulted in a mean edema score of 9.7 ± 7.8, whereas the observed T2w DIR-TSE edema scores were considerably lower compared to the observed LGE score (9.6 ± 7.6 vs. 15.3 ± 7.0, p < 0.0001; 9.7 ± 7.8 vs. 15.3 ± 7.0, p < 0.0001). Image artifacts were observed in 100 of 390 (25.6 %) acquired T2w DIR-TSE, and 24 LV segments were rated as not evaluable due to non-diagnostic image quality.

T2 mapping vs. T2w DIR-TSE
Compared to the current standard for myocardial edema imaging (T2w DIR-TSE), T2 mapping depicted myocardial edema in a considerably higher number of LV segments in both analyses (131 vs. 78, p < 0.0001; 134 vs. 76, p < 0.0001). Significantly higher true-positive (118 vs. 73, p < 0.0001; 110 vs. 76, p < 0.0001) and false-positive results (16 vs. 4, p = 0.037; 29 vs. 9, p = 0.033), as well as significantly lower false-negative (21 vs. 66, p < 0.0001; 29 vs. 72, p < 0.0001) and true-negative results (309 vs. 321, p = 0.031; 302 vs. 316, p = 0.024) were observed during segmental edema analyses for T2 mapping compared to T2w DIR-TSE. The edema scores derived from T2 mapping were significantly higher compared to the edema scores derived from the T2w DIR-TSE images in both analyses (17.7 ± 8.0 vs. 9.6 ± 7.6, p < 0.0001; 17.8 ± 9.1 vs. 9.7 ± 8.2, p < 0.0001). T2 mapping resulted in a significantly lower number of slices with image artifacts (3 vs. 100 / 0.6 % vs. 21.6 %, p < 0.0001) and in a significantly lower number of LV segments that were rated as non-evaluable (0 vs. 24, p = 0.012) compared to T2w DIR-TSE imaging.

Discussion

Even though T2 imaging of the myocardium has improved greatly during the past decades, myocardial edema imaging remains challenging in the clinical routine due to several limitations of the currently used T2-weighted dark-blood TSE sequences. These limitations include regional myocardial signal variation caused by phased array coils, bright rim artifacts from stagnant blood, and myocardial signal loss caused by through-plane motion [10 – 12]. Since several experimental and clinical studies have confirmed the great value of myocardial edema imaging in AMI [7, 19, 20] as well as in inflammatory cardiomyopathies [9], great efforts have been made to overcome the limitations of T2w dark-blood TSE imaging. Within the scope of these efforts, T2w bright-blood SSFP sequences have been developed within the last years [13, 21, 22]. Even though these approaches have addressed several of the mentioned shortcomings, these sequences are not common in the clinical routine presumably due to the fact that most of these techniques tend to provide a lower contrast between edematous and remote myocardium compared to T2-weighted dark-blood TSE images [23].

Nffenstein K et al. Cardiac MRI: T2-Mapping... Fortschr Röntgenstr 2014; 186: 166–172
Quantitative T2 mapping is a different approach for myocardial edema imaging that enables the differentiation of edematous from non-edematous myocardium by means of absolute values and not by differences in relative signal intensities. Even though multiple studies have reported myocardial T2 values over the past 25 years [24 – 26], T2 quantification has not been introduced into the clinical routine due to the fact that primarily spin-echo-based techniques, which are time-consuming and prone to motion artifacts, were used.

As shown in the present study, the employed edema imaging technique, which combines T2w SSFP imaging with T2 mapping, enables reliable generation of myocardial T2 maps within a single breath-hold in the clinical routine. Compared to the currently accepted clinical standard for myocardial edema imaging – T2w dark-blood TSE [8, 9] – this T2 mapping technique shows a remarkably lower frequency of visual image artifacts and a significant reduction in the number of LV segments with non-diagnostic image quality. These findings are in good agreement with the initial results from Giri et al., who demonstrated in healthy volunteers and a rather small number of patients (n = 3) that this T2 mapping technique is much less sensitive to motion artifacts than TSE imaging and is not sensitive to artifacts from slow-flowing blood [14]. However, it must be critically noted that the visual analysis of image artifacts in color-coded maps is more difficult than the detection of image artifacts in T2w dark-blood TSE images, so that it cannot be excluded that the frequency of artifacts in the T2 maps was underestimated in the present study.

Comparison of the T2 mapping approach to T2w dark-blood TSE imaging showed a considerably higher sensitivity for the detection of myocardial edema in the infarct zone (82.0 % vs. 50.4 %). Even though the most likely reason for this seems to be the fact that the utilized T2 mapping technique is much less sensitive to artifacts than TSE imaging, it also appears likely that visual assessment of color-coded T2 maps is easier than the reading of T2w dark-blood TSE images. While small alterations in the myocardial water content can be easily seen in T2 maps due to the chosen windowing of the color coding, in which small changes in the T2 values result in a distinct change in color, myocardial edema is more difficult to depict in T2w dark-blood TSE images due to the inherent low contrast between edematous and remote myocardium (Fig. 1 – 3).

Compared to previously published studies that found sensitivities of up to 100% [27] for the detection of myocardial edema in patients with AMI by T2w dark-blood TSE imaging, our reported sensitivity appears very low at first glance. On closer examination, however, it is evident that these differences are predominantly caused by different study designs. Whereas Friedrich et al. [27] reported a sensitivity of 100 % on a per-patient basis, the diagnostic accuracy in the present study was calculated on a per-segment basis, which enables a more detailed analysis. In a recently published study Payne et al. assessed the diagnostic performance of T2w dark-blood TSE for the detection of myocardial edema in AMI on a coronary artery perfusion territory basis. They found that T2w dark-blood TSE showed myocardial edema within the perfusion territory of the culprit coronary artery only in 61 % of cases [22].

Even though T2 mapping showed better sensitivity than T2w dark-blood TSE imaging, the sensitivity of T2 mapping is not perfect. A possible explanation for the somewhat limited sensitivity of T2 mapping might be the fact that T2 values in microvascular obstruction (MO) and remote myocardium are very similar (58.7 ±6 ms vs. 56 ± 3.4 ms [15]), which results in the fact that in the case of MO only the margin of the infarct shows higher T2 values compared to the remote myocardium. Since the spatial resolution of the T2 mapping approach is comparatively low due to constraints in the patients’ breath-holding capabilities, it is possible that in the case of extensive MO the thin non-MO infarct zone cannot be depicted due to partial volume effects.

Interestingly, the T2 mapping technique showed a slightly lower specificity than T2w dark-blood TSE imaging (94 % vs. 98 %) due to a statistically significantly higher number of false-positive results. One possible reason for this might be our definition of the standard of reference: LV segments were only rated as affected by AMI if a regional wall motion abnormality and/or an area of LGE in an ischemic pattern was present in an LV segment within the perfusion territory of the culprit vessel. However, it cannot be excluded that myocardial edema is the only sign of ischemic injury at the infarct border [20], which might have disadvantaged T2
mapping due to its higher sensitivity. However, the difference in the observed specificities is small and insignificant from a clinical point of view.

Our semiquantitative scoring showed fairly similar values for the extent of myocardial edema as assessed by T2 mapping and the extent of myocardial infarction as assessed by LGE. However, from previous studies it could have been expected that the T2 map edema score would be higher than the LGE score, since it has been shown that the edema zone is larger than the LGE zone in AMI [22, 28, 29]. However, the conflict between our findings and this expectation is only contrived. Since T2 mapping was not able to detect myocardial edema in all LV segments affected by AMI, the observed similar overall T2 map edema and LGE scores indicate that in LV segments with visible edema the edema zone was in fact larger than the LGE zone.

In the present study only visual analysis of the T2 maps was performed to detect edematous myocardium. Even though this approach foregoes the opportunity for automated edema detection, which is an obvious option in T2 mapping due to its quantitative character, visual analysis of the T2 maps will in all probability be the most common approach for the interpretation of T2 maps in the clinical routine. Therefore, detailed analysis of this approach is of great clinical interest, possibly even more so than analysis of the performance of automated edema detection algorithms. However, automated edema imaging is of clinical interest, too. Unfortunately, several facts might hinder automated edema deli-
neation in T2 maps, even though T2 mapping provides absolute values instead of relative signal intensities. As shown in the study by Giri et al. [14], the T2 mapping technique yields significantly higher T2 values in the apical segments compared to the basal and mid-ventricular segments when using short-axis T2 maps – possibly due to partial volume effects – which might hinder the use of a fixed threshold. Moreover, the graphic presentation of the mean T2 values of the infarct zone and in the remote myocardium in patients with AMI provided in the study by Verhaert et al. [15] demonstrated a certain overlap between these T2 values which might also hinder automated delineation of myocardial edema. Nevertheless, the development and validation of software algorithms for the automated detection of edematous myocardium in T2 maps is an interesting, although nontrivial, challenge for further studies.

Limitations

First of all, as mentioned above, the standard of reference used for the calculation of the diagnostic accuracy of both edema imaging approaches is not without limitation, which might have affected the calculated diagnostic accuracies. Moreover, since the present study focused on the diagnostic performance of T2 mapping in the clinical routine, it did not provide technical parameters like signal-to-noise ratios or T2 values of edematous and remote myocardium. However, these values have been investigated in detail previously [15], which relativizes this limitation.

Conclusion

The present study shows that the novel T2 mapping technique employed here allows the visualization of myocardial edema in AMI with a high sensitivity and specificity. This technique offers significantly better diagnostic accuracy in terms of a higher sensitivity as well as more robust image quality compared to the current standard for myocardial edema imaging, which is T2w dark-blood TSE imaging.

References

2 Wong DT, Richardson JD, Puri R et al. The role of cardiac magnetic resonance imaging following acute myocardial infarction. European radiology 2012; 22: 1757–1768
3 Achenbach S, Barkhausen J, Beer M et al. Consensus recommendations of the German Radiology Society (DRG), the German Cardiac Society (DGK) and the German Society for Pediatric Cardiology (DGPK) on the use of cardiac imaging with computed tomography and magnetic resonance imaging. Fortschr Röntgenstr 2012; 184: 345–368
7 Aletras AH, Tilak GS, Natanzon A et al. Retrospective determination of the area at risk for reperfused acute myocardial infarction with T2-weighted cardiac magnetic resonance imaging: histopathological and displacement encoding with stimulated echoes (DENSE) functional valida-
17 Wagner A, Mahrholdt H, Thomson L et al. Effects of time, dose, and inversion time for acute myocardial infarct size measurements based on magnetic resonance imaging-delayed contrast enhancement. Journal of the American College of Cardiology 2006; 47: 2027–2033
24 Bottomley PA, Foster TH, Argersinger RE et al. A review of normal tissue hydrogen NMR relaxation times and relaxation mechanisms from 1–100 MHz: dependence on tissue type, NMR frequency, temperature, species, excision, and age. Med Phys 1984; 11: 425–448
27 Friedrich MG, Abdel-Aty H, Taylor A et al. The salvaged area at risk in reperfused acute myocardial infarction as visualized by cardiovascular magnetic resonance. Journal of the American College of Cardiology 2008; 51: 1581–1587
29 Tilak GS, Hsu LY, Hoyt RF Jr et al. In vivo T2-weighted magnetic resonance imaging can accurately determine the ischemic area at risk for 2-day-old nonreperfused myocardial infarction. Invest Radiol 2008; 43: 7–15