Reference Values for Blood Flow Velocity in the Uterine Artery in Normal Pregnancies from 18 Weeks to 42 Weeks of Gestation Calculated by Automatic Doppler Waveform Analysis

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Abstract

Purpose: The goal of the present study was to establish new Doppler reference ranges for maternal heart rate, intensity-weighted mean blood flow velocities (Vmean) and impedance indices (PI, RI) for the uterine artery by automated waveform analysis.

Materials and Methods: A cross-sectional prospective study of 921 low-risk pregnancies was performed at 18–42 weeks of gestation. Uterine blood flow velocities were derived with pulsed-wave color Doppler. Measurements were carried out 1 to 2 cm above the crossing of the uterine and external iliac arteries. Reference ranges for the individual measuring parameters were constructed based on a growth function from a four-parameter class of monotonic continuous functions according to the smallest square principle.

Results: A significant increase in intensity-weighted mean uterine blood flow velocities was observed at 18–42 weeks of gestation (Vmean = 43 cm/s to 50 cm/s (p < 0.001)). Reference curves for the pulsatility and resistance indices (PI, RI) significantly decreased with progressing gestation (PI: 18 weeks: 0.89; 42 weeks: 0.65 and RI: 18 weeks: 0.45; 42 weeks: 0.35). No significant PI and RI differences were observed when different placental locations were compared. The maternal heart rate decreased from 88 bpm to 77 bpm.

Conclusion: Normal ranges for blood flow velocities and impedance indices in the uterine artery were established by Doppler ultrasound antenatal examinations of a large population of low-risk pregnancies. The data are proposed as reference curves to allow the early diagnosis of maternal and fetal risks.
Introduction

Doppler ultrasound measurements of the uteroplacental blood flow and its relevance for the early detection of gestational risks was first reported by Campbell et al. in 1983 [1]. Subsequent studies showed that a persistently increased pulsatility index throughout the second half of gestation and particularly the confirmation of a post-systolic notch in the uterine arteries were often accompanied by pregnancy-induced hypertension, preeclampsia, intrauterine growth restriction, placental abruption and intrauterine death [2–7].

Uterine Doppler measurements were predominantly performed using transvaginal sonography [8, 9] in the first half of gestation and by means of abdominal sonography in the second half of gestation [4, 5, 10]. Initially, Doppler velocimetry of the uterine artery was performed by continuous-wave measurements [3, 6, 11–13]. Pulsed Doppler spectral analysis [1, 7, 14] and Doppler color flow imaging techniques [4, 5, 10, 15] represented significant methodological improvements. In order to differentiate normal from pathological uterine waveforms, the definition of a normal range during pregnancy is very important. However, many reference ranges are associated with methodological flaws [16–18]. The validity of several reference ranges has been limited by small case numbers, the use of a single measuring parameter, longitudinal or cross-sectional studies, a short observation period, a lack of information about case numbers studied at the various time points from week 18 to 42 of gestation, differing techniques to obtain waveforms, differing sampling sites for Doppler measurements, calculation of raw data by inconsistently applied and inadequately explained mathematical methods, as well as by an insufficiently defined patient population.

Therefore, the present study intends to establish new Doppler ultrasound gestational age-dependent reference curves for the uterine artery (PI, RI, $V_{mean}$) in a normal obstetric population obtained by color Doppler measurements from the 18th to 42nd week of gestation. To this end, a mathematical growth model was developed by our group on the basis of validated methodological guidelines.

Patients and Methods

Doppler ultrasound examinations of the uterine artery were performed in a prospective cross-sectional study of 921 low-risk pregnancies, from 18–42 completed weeks of gestation. Every patient underwent only one examination. Gestational age was calculated from the last menstrual period, confirmed by first trimester crown-rump length measurement and corrected as required [19]. At the time of examination, the fetal abdominal and head circumference had to be within the 90% confidence interval of our standard curves [20]. An amniotic fluid volume within the normal range represented an additional inclusion criterion. Furthermore, only patients with normal findings regarding impedance indices (PI, RI) in the umbilical artery were included in the study. Smokers were required to abstain from smoking for at least two hours prior to examination. The exclusion criteria included: intrauterine growth restriction, hypertensive diseases, preeclampsia, maternal coagulation disease, diabetes, collagen vascular disease, pharmacotherapy and drug dependence, uterine malformations, labor activity and maternal emotional states. Further uterine Doppler flow waveforms with the presence of a unilateral or bilateral post-systolic notch were excluded. The ultrasound investigations were performed with a 2–5 MHz broadband transducer and a 2.25 MHz transducer (Combison 530/530 MT, Kretz-Technik, Austria and Voluson 730 expert GE Medical systems) was used to derive the blood flow velocities. The ultrasound transducer was positioned on the lower lateral side of the abdomen. Color Doppler imaging was performed to visualize the uterine artery and optimize the insonation by pulsed-wave Doppler (Fig. 1, 2). Uterine flow velocities were recorded from the arteries using color Doppler flow imaging and normal Doppler velocity waveforms of the uterine artery were obtained (Fig. 2).

Fig. 1 Color flow imaging shows the complex uterine circulation in the lower lateral abdominal quadrant.

Abb. 1 Farbdopplersonografische Darstellung des uteroplazentaren Kreislauf im lateralen unteren Quadranten des Abdomens.

Fig. 2 Transabdominal color flow imaging and normal Doppler velocity waveforms of the uterine artery.

Abb. 2 Transabdominale farbdopplersonografische Darstellung eines normalen uterinen Dopplerflussspektrums.
Flow velocities were taken approximately 1 cm to 2 cm above the crossover of the external iliac artery on both sides (Fig. 2). Doppler measurements were performed according to the guidelines of the International Perinatal Doppler Society [21]. Only patients with an anterior, posterior or fundal location of the placenta were examined. The mean PI, RI and \( V_{\text{mean}} \) of the right and left uterine artery were calculated. The pulse repetition frequency ranged from 4 to 6 kHz and the wall filter was set at 120 Hz. The angle of insonation was below 30° for all measurements. Calculations for 3 uniform heart cycles were made from the stored image using an automatic waveform analysis integrated into the ultrasound device. The pulsatility and resistance indices (PI, RI), intensity-weighted mean velocity (\( V_{\text{mean}} \)) and maternal heart rate (MHR) were calculated automatically from the mean values. The spatial average intensity for color and pulsed Doppler was consistently less than 100 mW/cm². All measurements were performed by one investigator (F.B.) with extensive Doppler sonography experience.

Statistical method for creating age-dependent reference percentiles

Reference ranges for the respective gestational weeks were determined with the aim of creating smoothened growth curves for the entire gestational period. For this purpose, the statistical method suggested by Wellek et al. (1995) was used and is briefly described below [22]:

1. The boundaries of the bands were shown as smoothed curves instead of as step or piece-wise linear functions.

2. The central line of the band was determined by fitting a non-linear regression function derived from a sufficiently flexible class of monotonic functions parametrized as parsimoniously as possible. The following model describes a class of monotonic functions which proved to be very well-suited for this purpose:

\[
g(t) = c \times (d + I_x(t - t_1))(a,b),
\]

where \( t_1 \) and \( t_2 \) denote the upper limit of the time range, respectively, and \( I_x(a,b) \) stands for the value of the beta distribution function with parameters \( (a,b) \) at \( x \), for any point \( x \) in the unit interval \((0,1)\). Of the four parameters involved in the model, the first two, i.e., \( a \) and \( b \) determine the form of the curve, while \( c \) and \( d \) reflect the scale and order of magnitude. In addition, the sign of \( c \) coincides with that of the slope of the curve.

3. The boundary curves were determined so that the width of the band increases or decreases linearly from left to right according to the ratio of the conditional standard deviations observed in the first and the last decile with respect to gestational age. For the majority of the measurements analyzed in this paper, variability increased with the observation time points leading to increasing bandwidths.

4. Subject to condition (III), the smallest bandwidth was computed to provide a minimum coverage of 90% for the individual observations contained in the reference sample. In nonsymmetrical cases, the proportion of points outside the band is controlled separately for the lower and the upper part, in order to obtain (approximate) equality of tails. In other words, in all diagrams and tables, the lower and upper boundaries correspond as closely as possible to the 5th and 95th percentiles, respectively. This obviously entails more or less marked differences between the upper and the lower reference curves with respect to the distance from the regression line.

Results

In 921 cases good Doppler flow spectra were derived from the left and right uterine artery. The ranges are shown in Figs. 3–6 and Table 1 and 2. The reference curve of the pulsatility index (PI) is characterized by a linear pattern, showing a decrease of 0.89 to 0.65 from the 18th–42nd week of gestation. A similar pattern was observed for the resistance index (RI) with a decrease of 0.45 to 0.35. The maternal heart rate decreased from 88 bpm in the 18th week to 77 bpm in the 42nd week of gestation.

With regard to intensity-weighted mean blood flow velocities (\( V_{\text{mean}} \)), an increase of 43 to 50 cm/s was noted for the observa-

![Fig. 3](image1)

**Fig. 3** Individual measurements and calculated reference ranges for the pulsatility index (PI) in the uterine artery. The standard boundaries include 90% of the normal patient population.

**Abb. 3** Darstellung der Einzelmessungen für den Pulsatilitätsindex (PI) der A. uterina. Das Konfidenzintervall beinhaltet 90% des Normalkollektivs.

![Fig. 4](image2)

**Fig. 4** Individual measurements and calculated reference ranges for the resistance index (RI) in the uterine artery. The standard boundaries include 90% of the normal patient population.

**Abb. 4** Darstellung der Einzelmessungen für den Resistenzindex (RI) der A. uterina. Das Konfidenzintervall beinhaltet 90% des Normalkollektivs.
The regression models fitted to the data of the variables under consideration are summarized in Table 3. The impedance indices for the placental positions (anterior, posterior, fundal) were compared in 10 patients and showed no significant differences. Comparisons of our reference values with the results of the literature and are presented for the pulsatility index (PI) and resistance index (RI) were performed with the results of the literature and are presented in Fig. 7, 8.

Discussion

The present study examined parameters of uterine blood flow velocity and impedance indices as well as the maternal heart rate in a large, well-defined low-risk population of pregnancies. Evaluation of 921 women between the 18th and 42nd week of pregnancy demonstrated a significant increase in the blood flow velocity ($V_{\text{mean}}$) of the uterine artery and significant decreases of uterine resistance indices (PI, RI) as well as a decrease of the maternal heart rate.

<table>
<thead>
<tr>
<th>Gestational age (wks)</th>
<th>Mean $^1$</th>
<th>PI $90%$ interval</th>
<th>Mean $^1$</th>
<th>RI $90%$ interval</th>
<th>Mean $^1$</th>
<th>$V_{\text{mean}}$ $90%$ interval</th>
</tr>
</thead>
<tbody>
<tr>
<td>18</td>
<td>0.888</td>
<td>(0.509 – 1.407)</td>
<td>0.447</td>
<td>(0.222 – 0.659)</td>
<td>43.458</td>
<td>(20.659 – 71.901)</td>
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<td>0.838</td>
<td>(0.460 – 1.356)</td>
<td>0.429</td>
<td>(0.204 – 0.641)</td>
<td>44.025</td>
<td>(21.202 – 72.500)</td>
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<td>20</td>
<td>0.812</td>
<td>(0.436 – 1.328)</td>
<td>0.419</td>
<td>(0.194 – 0.630)</td>
<td>44.831</td>
<td>(21.982 – 73.337)</td>
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<td>21</td>
<td>0.795</td>
<td>(0.420 – 1.309)</td>
<td>0.411</td>
<td>(0.186 – 0.622)</td>
<td>45.704</td>
<td>(22.830 – 74.240)</td>
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<td>22</td>
<td>0.781</td>
<td>(0.407 – 1.293)</td>
<td>0.405</td>
<td>(0.180 – 0.615)</td>
<td>46.545</td>
<td>(23.647 – 75.113)</td>
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<td>23</td>
<td>0.769</td>
<td>(0.397 – 1.280)</td>
<td>0.400</td>
<td>(0.175 – 0.610)</td>
<td>47.301</td>
<td>(24.377 – 75.899)</td>
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<td>24</td>
<td>0.759</td>
<td>(0.388 – 1.268)</td>
<td>0.395</td>
<td>(0.171 – 0.605)</td>
<td>47.945</td>
<td>(24.997 – 76.575)</td>
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<td>25</td>
<td>0.751</td>
<td>(0.381 – 1.258)</td>
<td>0.391</td>
<td>(0.167 – 0.601)</td>
<td>48.473</td>
<td>(25.500 – 77.133)</td>
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<td>26</td>
<td>0.743</td>
<td>(0.374 – 1.248)</td>
<td>0.387</td>
<td>(0.163 – 0.597)</td>
<td>48.889</td>
<td>(25.891 – 77.580)</td>
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<tr>
<td>27</td>
<td>0.736</td>
<td>(0.369 – 1.239)</td>
<td>0.384</td>
<td>(0.160 – 0.593)</td>
<td>49.206</td>
<td>(26.183 – 77.928)</td>
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<td>28</td>
<td>0.729</td>
<td>(0.363 – 1.230)</td>
<td>0.380</td>
<td>(0.157 – 0.590)</td>
<td>49.439</td>
<td>(26.391 – 78.192)</td>
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<td>29</td>
<td>0.722</td>
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<td>0.378</td>
<td>(0.154 – 0.587)</td>
<td>49.604</td>
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<td>30</td>
<td>0.716</td>
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<td>0.375</td>
<td>(0.152 – 0.584)</td>
<td>49.716</td>
<td>(26.619 – 78.532)</td>
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<td>(0.144 – 0.574)</td>
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<tr>
<td>35</td>
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<td>0.364</td>
<td>(0.142 – 0.571)</td>
<td>49.886</td>
<td>(26.664 – 78.856)</td>
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<tr>
<td>36</td>
<td>0.684</td>
<td>(0.330 – 1.171)</td>
<td>0.362</td>
<td>(0.140 – 0.569)</td>
<td>49.889</td>
<td>(26.643 – 78.891)</td>
</tr>
<tr>
<td>37</td>
<td>0.679</td>
<td>(0.326 – 1.164)</td>
<td>0.360</td>
<td>(0.139 – 0.567)</td>
<td>49.891</td>
<td>(26.620 – 79.232)</td>
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<tr>
<td>38</td>
<td>0.674</td>
<td>(0.322 – 1.157)</td>
<td>0.358</td>
<td>(0.137 – 0.566)</td>
<td>49.891</td>
<td>(26.595 – 79.955)</td>
</tr>
<tr>
<td>39</td>
<td>0.669</td>
<td>(0.318 – 1.150)</td>
<td>0.357</td>
<td>(0.136 – 0.564)</td>
<td>49.891</td>
<td>(26.571 – 79.986)</td>
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<tr>
<td>40</td>
<td>0.663</td>
<td>(0.313 – 1.143)</td>
<td>0.355</td>
<td>(0.135 – 0.562)</td>
<td>49.891</td>
<td>(26.546 – 79.017)</td>
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<td>41</td>
<td>0.657</td>
<td>(0.308 – 1.134)</td>
<td>0.354</td>
<td>(0.134 – 0.561)</td>
<td>49.891</td>
<td>(26.521 – 79.048)</td>
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<td>42</td>
<td>0.649</td>
<td>(0.302 – 1.125)</td>
<td>0.353</td>
<td>(0.133 – 0.559)</td>
<td>49.891</td>
<td>(26.496 – 79.079)</td>
</tr>
</tbody>
</table>

$^1$ Smoothed by means of nonlinear regression.
These alterations are in part the result of the physiological trophoblastic invasion of the spiral arteries and the loss of the musculoelastic coat of the arteries and are in part caused by an increased cardiac output, a decrease of blood viscosity and a gradual reduction of the peripheral vascular resistance in the maternal compartment [23, 24].

The trophoblastic invasion in the first half of gestation proceeds in two phases and causes pronounced hemodynamic changes in the uteroplacental circulation including the reduction of resistance in the uterine vessels. In the second half of gestation, the process of placentation is largely completed which we found to be reflected by only marginal changes in the impedance indices (PI, RI). These observations are consistent with the literature [1, 10, 11, 25, 26]. Thus, uterine Doppler waveform measurements are similar regardless of the differing Doppler technologies applied.

In order to establish valid reference curves, it is important to provide standardized and reproducible measurements of uterine blood flow velocity combined with an exact definition of the sampling site and assessment of the placenta location [10, 27]. Bewley et al. demonstrated a reduction of impedance indices along the uterine artery with increasing distance from the crossing of the uterine and external iliac arteries [27]. This may well be explained by the complexity of the uterine collateral vasculature.

In addition, the location of the placenta may have considerable influence on uterine blood flow [10, 27]. Therefore, we only included measurements in which the placenta location was anterior, posterior or fundal within the uterus. Bower et al. showed significant differences in impedance indices of the uterine artery depending on the site of placentation [10]. Significantly lower PI and RI values were found at the site of placental adherence in comparison to the contralateral side [10, 26, 27]. Although Bewley et al. reported lower resistance indices of the uterine artery when the placenta was located in an anterior position compared to posterior placentation, we were unable to confirm this [27]. A possible explanation could be the use of continuous-wave Doppler in their study, which did not allow standardized reproducible derivation of the uterine blood flow velocity. Even though the uterine blood flow velocity can be measured by continuous-wave Doppler (CW) or pulsed Doppler analysis, only color Doppler ultrasound permits standardized and reproducible derivation of the uterine blood flow velocity. The latter technique has the advantage of allowing accurate localization of the uterine artery with standardized alignment of a low angle...
of insonation and exact positioning of the sample volume [4, 15].

Uterine reference curves with a similar study design and the same examination technique were created by Gomez et al. for the pulsatility index and by Kurmanavicius et al. for the resistance index [25, 26]. In contrast to these studies, we excluded pregnancies with a unilateral or bilateral post-systolic notch and the placenta in a lateral position within the uterus. Additionally, our data were collected by a single individual while several examiners participated in the collection of data in the other two studies. However, this does not seem to be of great relevance as the interobserver variability is only marginal [27, 28]. Comparison of our reference ranges of the uterine artery to collectives of similar size and homogeneity shows a nearly identical curve progression for the pulsatility index as well as the resistance index [25, 26]. In comparison to our data, the reference curves published by Kurmanavicius et al. exhibit a marginally narrower confidence interval and slightly increased resistance indices during the entire gestational period, while Gomez et al. feature a wider confidence interval and higher pulsatility and preeclampsia indices during the entire gestational period, while originally narrower confidence interval and slightly increased resistance indices between the 18th and 24th week of gestation [25, 26]. This could be explained by our exclusion of pregnancies with a unilateral or bilateral post-systolic notch, thus resulting in slightly lower impedance indices. Differing statistical calculation could be a further reason for minor deviations [16, 17, 22, 29].

The evaluation of pathological unilateral or bilateral uterine Doppler waveforms is qualitatively estimated by impedance indices (PI, RI) and demonstration of the post-systolic notch [3, 7, 15]. The latter is viewed as a risk factor for the development of intrauterine growth restriction, pregnancy-induced hypertension and preeclampsia as well as for intrauterine death and a higher placental abruption rate [2–4, 30]. Although detection of a bilateral notch is associated with a higher complication rate during pregnancy, knowledge of the normal limits of uterine impedance indices is equally important to differentiate normal from pathological pregnancies and for their prognostic assessment. Therefore, accurately constructed reference curves in a well-defined low-risk patient collective are required. A recently conducted bivariable meta-analysis showed that an increased pulsatility index associated with a post-systolic notch in the second trimester of pregnancy has a high predictive value for the development of preeclampsia in a low-risk as well as in a high-risk patient collective [31]. However, the predictive value was lower for intrauterine growth restriction [31]. For the future a combination of biochemical markers with ultrasonographic markers represents a promising approach to improve the prediction of preeclampsia in the first as well as the second trimester of pregnancy [32].

In summary, the present study provides reference curves for the impedance indices (PI, RI), Vmean, and the maternal heart rate in a large well-defined low-risk patient collective and shows similar curve progression compared to the literature. The present reference curves can be applied to the evaluation of uterine blood flow velocity and impedance indices when the placenta is located in a central position.

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