# Workload and Injury in Professional Soccer Players: Role of Injury Tissue Type and Injury Severity

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#### Key words

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#### **Bibliography**

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#### **ABSTRACT**

The purpose of the present study was to examine the influence of workload prior to injury on injury (tissue type and severity) in professional soccer players. Twenty-eight days of retrospective training data prior to non-contact injuries (n = 264) were collated from 192 professional soccer players. Each injury tissue type (muscle, tendon and ligament) and severity (days missed) were categorised by medical staff. Training data were recorded using global positioning system (GPS) devices for total distance (TD), high speed distance (HSD, > 5.5 m/s<sup>-1</sup>), and sprint distance (SPR, >7.0 m/s<sup>-1</sup>). Accumulated 1, 2, 3, 4-weekly loads and acute:chronic workload ratios (ACWR) (coupled, uncoupled and exponentially weighted moving average (EWMA) approaches) were calculated. Workload variables and injury tissue type were compared using a one-way ANOVA. The association between workload variables and injury severity were examined using a bivariate correlation. There were no differences in accumulated weekly loads and ACWR calculations between muscle, ligament, and tendon injuries (P>0.05). Correlations between each workload variable and injury severity highlighted no significant associations (P>0.05). The present findings suggest that the ability of accumulated weekly workload or ACWR methods to differentiate between injury type and injury severity are limited using the present variables.

# Introduction

Soccer is a complex contact sport with high physical, technical, and tactical demands at the elite level [1]. Barnes et al. [2] highlighted the ever-increasing high-intensity demands of professional soccer in the modern game, with an increase in sprint distance of ~35% over a 7-season period. Because of the intense physical nature of the sport, a high level of injuries has been reported across a range of professional clubs [3]. In particular, non-contact muscular injuries appear to be a significant issue for both coaching and medical staff, accounting for almost one third of all time-loss injuries in

men's professional soccer [4, 5]. Financially, the average cost of a first-team player in a professional team being injured for 1 month is calculated to be worth around €500 000 [6]. Despite the increased body of knowledge and applied injury prevention strategies around non-contact injuries within soccer, the rate of these types of injuries continues to rise [7].

Within professional soccer, it is commonplace for sport science staff to monitor a range of variables across the training programme [8]. The monitoring of training load (TL) on a daily basis is now standard practice in order to help facilitate the prescription of the

correct 'dose' of TL to maximise adaptation and minimise injury risk. Measures of TL can be categorized into either external (i. e., exercise prescription by the coach) or internal (i. e., physiological stress imposed on the players) [9]. The evolution in the accessibility of wearable technology within soccer has led to the widespread use of global positioning systems (GPS) to quantify athlete movements during training and match play [8]. Common measures collected and monitored in elite soccer include high-speed distance covered ( $>5.5\,\text{m/s}^{-1}$ ), acceleration/deceleration efforts, and estimated metabolic power [8]. Sports science and medical practitioners can subsequently create individualised monitoring strategies based on the GPS data to feed back information to ensure observed TL is compliant with the training planned by the coaches.

Elite-level soccer players typically sustain two injuries per season, resulting in 50 injuries within a squad of 25 players [4]. It has been previously suggested that the incorrect application of workload can act as an external risk factor for injury in athletes [10]. In particular, a sudden increase in the TL placed upon an athlete (i.e., 'spike') [11] or insufficient chronic TL stimulus [12] can contribute to an increased injury risk in athletes. There has been growing use of the acute:chronic workload ratio (ACWR) in order to monitor and prescribe appropriate TLs in athletes [13]. The calculation involves the assessment of the current 1-week workload (acute) relative to the chronic workload (typically 2, 3, or 4-weekly average) [5]. Previous research has used a combination of ACWR and/or accumulated weekly TLs to investigate the relationship with injury across a range of sports, including: rugby [14–19], Australian rules football (AFL) [20-26], American football [27, 28], handball [29], Gaelic football [30], and soccer [12, 31–37]. Despite this growing body of research, there have been conflicting findings within the literature. One of the reasons may be due to the range of ways in which the ACWR can be calculated. Lolli et al. [38] argue the rolling average ACWR calculation can produce spurious correlations, which can be explained by mathematical coupling, whereas others suggest that calculating the ACWR using exponentially weighted moving averages (EWMA) could provide a more sensitive model to inform decision-making [22]. To avoid error associated with ratios, researchers have also compared the cumulative totals for each variable [35]. To the authors' knowledge, few studies have calculated and compared all of the above approaches using the same training data [22, 39].

Within soccer, each type of non-contact injury has its own unique incidence rate and severity [40]. For example, anterior cruciate ligament injuries typically occur once every 10 000 h of training and cause a player to be withdrawn from training for around 200 days [41]. Muscle injuries happen more often (~1 per 1 000 h) and cause the player to be removed from training and competition for around 24 days [40]. Previous studies investigating the TL preceding injury have combined all non-contact injuries without distinguishing between the tissue type (e.g., tendon) and the influence of injury severity. Collating training data for each type of injury might improve our understanding of why players sustain particular injuries. If, for example, the ratio of sprinting is different prior to muscle injuries when compared to tendon or ligament injuries, this could help inform our understanding of how the musculoskeletal system responds to the training currently employed by professional soccer teams. This could also inform the decisionmaking processes which assist how we prescribe training and implement risk management plans to reduce injury.

Therefore, the purpose of the present study was to examine the relationships of accumulated workloads, the ACWR using different methods, and injury occurrence (severity and tissue type) in a large cohort of professional soccer players.

# Materials and Methods

#### **Participants**

Data were collected from professional soccer players (n = 192) from 8 teams competing in recognised Union of European Football Associations (UEFA) leagues. Twenty-eight days of retrospective training and injury data were collected across both the 2015/2016 and 2016/2017 seasons. All clubs and players provided written informed consent to participate in the study, which was approved by the Institutional Review Board (IRB) at Liverpool John Moores University (United Kingdom) and conformed to the recommendations of the Declaration of Helsinki and those outlined by Harriss and colleagues [42]. Goalkeepers were excluded from the study due to the different nature of their playing activity.

## Quantifying workload

Training load was quantified using GPS data collected from all onpitch training sessions and matches during the in-season phase (Optimeye S5, firmware version 717, Catapult Sports, Melbourne, Australia). Each player was assigned their own specific device in order to avoid potential inter-unit reliability error [43]. The device was worn inside a custom-made vest supplied by the manufacturer that was positioned across the scapula of the players. The number of satellites and horizontal dilution of position (HDOP) across all data collections were 14.0 ± 2 and 0.77 ± 0.03, respectively. The Catapult S5 GPS device has previously shown acceptable levels of both reliability [44] and validity [45] for velocity-based variables. The data collection procedures followed the guidelines for using GPS data in sport [43]. Following each session, data were downloaded by a member of each sports science team using the manufacturer's software (Openfield, version 1.14, Catapult Sports, Melbourne, Australia). The following variables were included for data analysis: total distance (TD), high-speed distance (HSD,  $> 5.5 \,\text{m/s}^{-1}$ ), and sprint distance (SPR,  $> 7.0 \,\text{m/s}^{-1}$ ). The minimum effort duration for velocity-based variables was set at 0.4 secs in line with previous recommendations [46].

#### Injury quantification

Injury information was recorded using the clubs' standardised internal medical procedures and were guided by the Munich Consensus statement [47]. Non-contact injury was defined as an injury that involved no physical contact from another player and resulted in absence from participation in training with the normal group of players. Within each club, medical doctors and qualified physiotherapists diagnosed and recorded each injury tissue type (muscle, tendon, or ligament) confirmed using ultrasound technology [47]. Only injuries that were sustained for the first time were included in the final analysis. As such, data for subsequent recurring injuries were excluded. The severity of each injury was quantified as the number of days missed from training with the main group of 'starting' players, involving full

intensity and contact. The severity of each injury was also classified as either minimal (1–3 days missed), mild (4–7 days missed), moderate (8–28 days missed), or severe (>29 days missed) [32]. All injury data were stored in a central database and then sent to the researchers via an encrypted platform.

### Data analyses

Data were categorised into 7-day blocks (weeks) starting with the most recent day to the injury occurrence regardless of the week day. Accumulated 1, 2, 3, 4-weekly loads were subsequently calculated using the sum of the daily load across the previous week(s). ACWRs were calculated using the GPS-derived data collected across the 28-day period prior to each injury. The last session recorded before the injury was classified as 'day 1'. From this day, the data were categorised into 7-day phases using a rolling average approach prior to this point (regardless of the day of the week). The acute training load was defined as the average 'load' for the 7 days prior to the injury. Both 'coupled' (C) and 'uncoupled' (UC) ACWRs were calculated [52]. As a result, the chronic aspect of the ratio included either: a) the average of the 2<sup>nd</sup> and 3<sup>rd</sup> week prior to the injury (UC ACWR 1:3); b) the 2<sup>nd</sup>, 3<sup>rd</sup>, and 4<sup>th</sup> week prior to injury (UC ACWR 1:4); c) the average of the 1st, 2nd and 3rd week prior to the injury (C ACWR 1:3); or d) the 1st, 2nd, 3rd, and 4th week prior to injury (C ACWR 1:4). In addition, the exponentially weighted ACWR was calculated according to the equation outlined by Williams and colleagues [48].

#### Statistical analysis

The software package SPSS (Version 24.0 SPSS Inc. Chicago, IL, USA) was used to conduct the statistical analysis. Prior to statistical comparisons, assessments for normality and variance assurance were made. A one-way analysis of variance (ANOVA) was subsequently used to determine whether there are any statistically significant differences between the means of each injury tissue type (muscle, tendon, and ligament) and each accumulated weekly load, coupled, uncoupled, EWMA (1:3 and 1:4), for TD, HSD and SPR. To examine the relationship between ACWR method and weekly accumulated workload on injury severity, correlations were performed using a bivariate analysis. The level of significance was set at P<0.05. Confidence intervals (95 % CI) are provided alongside descriptive data (mean ± standard deviation (SD)).

# Results

Two hundred and sixty-four non-contact injuries from eight professional teams were collected. One hundred and forty injury data sets were excluded due to inconsistent and/or missing data. Therefore, 124 lower limb injuries were included in the final analysis

(muscle, n = 79; tendon, n = 28; ligament, n = 17). Descriptive data for each injury is presented in  $\triangleright$  **Table 1**.

#### Influence of ACWR on injury tissue type and severity

Workload data for each ACWR method in relation to injury tissue type and severity are presented in ► **Table 2**. Regardless of the ACWR method used, there was no significant difference shown between injury tissue type for all workload variables (P>0.05). In addition, there was no relationship found between ACWR methods and injury severity (P>0.05).

# Influence of accumulated weekly workload on injury tissue type and severity

Workload data for the different accumulated weekly loads in relation to injury tissue type and severity are presented in ▶ **Table 3**. There was no significant relationship found across the different accumulated weekly workload calculations (1, 2, 3, and 4-weekly loads) and injury tissue type for all workload variables (P>0.05). In addition, there was no relationship found between accumulated workloads and injury severity (P>0.05).

#### Discussion

The purpose of the present study was to examine the relationships of accumulated workloads, the ACWR using different methods, and injury occurrence (severity and tissue type) in a large cohort of professional soccer players. Regardless of the ACWR method used or weekly accumulated workloads, there was no observed differences in workload variables and each injury tissue type. In addition, there was no relationship found between workload variables and injury severity. The present findings suggest that workload data typically used by professional soccer teams may not be able to discriminate between injury type and/or severity.

The relationship between the ACWR and injury risk in soccer has been previously examined in the literature [12, 30–32, 34–36, 49]. However, limited attention has been given to the ability of the ACWR to differentiate between different tissue types within noncontact injuries. Understanding if the different workloads associated with the training programme could result in each type of injury and might have practical relevance for coaches who aim to minimise the injury burden within their team. The present study highlighted that the workload exposure across both ACWR methods and accumulated weekly loads were not different before either a muscle, tendon, or a ligament injury. Considering that muscles, tendons, and ligaments have unique mechanical intensity thresholds that initiate distinct temporal responses [50], it is logical to suggest that each injury could have its specific loading pattern prior to the injury [51]. Indeed, previous research has noted that an acute

▶ **Table 1** Descriptive information for injury incidence across all clubs.

		Injur		Injury environment				
	1–3 d Minimal	4–7 d Mild	8–28 d Moderate	>29 d Severe	Match	Training		
Muscle	18	18	33	10	30	49		
Ligament	0	0	0	17	0	17		
Tendon	4	9	11	4	10	18		

▶ Table 2 EWMA, coupled and uncoupled ACWR data for muscle, ligament, and tendon injures.

		95% Confidence Interval (lower – upper)		Min		Max Range	One-Way ANOVA		Effect	Correlation	
	Mean±SD				IVIAX		F P		Size (η²)	Pearson Sig	
EWMA ACWR TD											
Muscle	1.03 ± 0.27	0.96	1.09	0.13	1.65	1.52			0.007		
Ligament	0.95 ± 0.33	0.77	1.12	0.53	1.88	1.35	0.43	0.663		-0.055	0.542
Tendon	1.01 ± 0.24	0.91	1.10	0.56	1.60	1.04	1				
EWMA ACWR HSD											
Muscle	0.95 ± 0.29	0.88	1.01	0.12	1.66	1.55					
Ligament	1.00 ± 0.39	0.79	1.21	0.42	1.75	1.32	0.17	0.898	0.002	0.031	0.732
Tendon	0.99±0.36	0.85	1.13	0.55	2.16	1.61	1				
EWMA ACWR SPR											
Muscle	0.93 ± 0.42	0.83	1.03	0.12	2.07	1.95					
 Ligament	0.99 ± 0.57	0.68	1.29	0.12	1.98	1.86	0.09	0.924	0.001	0.013	0.888
Tendon	0.98 ± 0.51	0.78	1.18	0.08	2.22	2.14					
1:4 ACWR [C] TD											
Muscle	1.06 ± 0.32	0.99	1.14	0.20	1.96	1.76					
Ligament	1.04±0.35	0.85	1.22	0.59	2.23	1.64	0.2	0.819	0.003	-0.016	0.861
Tendon	1.03 ± 0.36	0.89	1.18	0.36	2.18	1.82	1				
1:4 ACWR [C] HSD	1		-		1						
Muscle	0.99±0.39	0.90	1.09	0.02	2.26	2.23					
Ligament	1.08 ± 0.30	0.92	1.23	0.58	1.57	0.99	0.16	0.856	0.003	0.010	0.911
Tendon	1.07 ± 0.46	0.89	1.25	0.23	2.64	2.41	-				
1:4 ACWR [C] SPR	1107 = 0110	0.03	1.123	0.23							
Muscle	1.07 ± 0.66	0.91	1.22	0.00	2.87	2.87					
Ligament	1.14±0.66	0.79	1.49	0.12	2.72	2.59	0.38	0.721	0.005	0.038	0.678
Tendon	1.01 ± 0.61	0.77	1.25	0.00	2.64	2.64	- 0.50			0.030	0.070
1:3 ACWR [C] TD	1.01 = 0.01	0.77	1.23	0.00	2.04	2.04					
Muscle	1.06±0.30	0.99	1.13	0.23	2.12	1.89		0.596	0.009	0.006	0.943
Ligament	1.07 ± 0.24	0.94	1.19	0.60	1.69	1.03	0.52				
Tendon	1.00 ± 0.24	0.89	1.11	0.38	1.92	1.54	0.52				
1:3 ACWR [C] HSD	1.00±0.28	0.89	1.11	0.36	1.32	1.54					
Muscle	0.99±0.37	0.91	1.08	0.03	1.96	1.93					
	-	0.91	1.08	0.03			0.12	0.894	0.002	0.014	0.877
Ligament	1.09 ± 0.23			<u> </u>	1.55	0.83	0.12				
Tendon	1.04±0.37	0.89	1.18	0.27	2.31	2.04					
1:3 ACWR [C] SPR	1.05 + 0.63	0.02	1.20	0.00	2.66	2.66					
Muscle	1.06 ± 0.62	0.92	1.20	0.00	2.66	2.66	0.64	0.511	0.011	0.034	0.710
Ligament	1.13±0.55	0.84	1.42	0.22	2.06	1.84	0.64			0.034	0.710
Tendon	0.96 ± 0.51	0.75	1.16	0.00	2.37	2.37					
1:4 ACWR [UC] TD	0.50 : 0.35	0.45	0.56	0.05	1.00	1 77					
Muscle	0.50 ± 0.25	0.45	0.56	0.06	1.83	1.77	- 17	0.000	0.005	0.155	0.082
Ligament	0.53 ± 0.51	0.26	0.80	0.22	2.38	2.16	0.17	0.898	0.005	-0.157	
Tendon	0.52 ± 0.30	0.40	0.63	0.13	1.36	1.23					
1:4 ACWR [UC] HSD			1			1.0-					
Muscle	0.48 ± 0.30	0.41	0.55	0.01	1.85	1.85	4	0.452	0.013	-0.032	0.729
Ligament	0.55±0.33	0.37	0.72	0.20	1.51	1.31	0.78				
Tendon	0.57 ± 0.48	0.38	0.75	0.08	2.27	2.20					
1:4 ACWR [UC] SPR											
Muscle	0.63 ± 0.66	0.47	0.78	0.00	3.66	3.66	1				
Ligament	0.79 ± 1.08	0.22	1.37	0.03	4.56	4.52	0.56	0.604	0.008	-0.051	0.576
Tendon	$0.58 \pm 0.50$	0.38	0.77	0.00	1.95	1.95					

▶ Table 2 Continued.

		95% Confidence Interval			1		One-Way ANOVA		Effect	Correlation	
	Mean ± SD	(lower –	upper)	Min	Max	Range	F	Р	Size (η²)	Pearson	Sig.
1:3 ACWR [UC] TD											
Muscle	0.89 ± 0.42	0.79	0.98	0.10	2.32	2.22		0.942	0.001	-0.101	0.262
Ligament	0.86 ± 0.45	0.62	1.10	0.37	2.38	2.01	0.06				
Tendon	0.86 ± 0.51	0.65	1.06	0.20	2.79	2.58					
1:3 ACWR [UC] HSD											
Muscle	0.84±0.46	0.74	0.95	0.01	2.13	2.12		0.901	0.002	-0.049	0.596
Ligament	0.95 ± 0.41	0.73	1.17	0.38	1.80	1.42	0.14				
Tendon	0.96 ± 0.84	0.63	1.29	0.14	4.16	4.02	1				
1:3 ACWR [UC] SPR											
Muscle	1.26 ± 1.46	0.93	1.60	0.00	7.67	7.67	0.63	0.522	0.011	-0.044	0.640
Ligament	1.21 ± 1.07	0.65	1.78	0.10	4.56	4.46					
Tendon	0.94±0.75	0.64	1.23	0.00	3.58	3.58					

**Abbreviations:** EWMA, exponentially weighted moving average; ACWR, acute chronic ratio; TD, total distance; HSD, high-speed distance; SPR, sprint distance; C, coupled; UC, uncoupled; ACC, accumulative; η², eta squared.

increase in sprinting is associated with muscle-based injuries [12]. This is supported by experimental research which demonstrates the transfer of force from ground to bone, from bone to tendon, and from tendon to muscle is higher during sprinting actions [52]. It was anticipated that muscle injuries would have occurred in individuals who underwent a 'spike' in sprint-based activity in the week before the injury [31, 32]. However, our results highlight that the training data for each player is homogeneous regardless of the type of injury. We also observed no differences in the ACWR (i. e., coupled, uncoupled or EWMA) for each of the workload measures included in this study (total distance, high speed distance, and sprint distance) across each injury tissue type. This suggests that the exposure to use of the ACWR and accumulated weekly loads may not be sensitive enough to detect differences in non-contact injury tissue types in professional soccer players.

It is possible that the lack of differences observed in ACWR between each injury tissue type could be partly explained by the workload variables examined in the present study. Soccer training and match play include an array of sport-specific skills (e.g., dribbling, passing, and shooting) interspersed with repeated explosive activities and movements (e.g., high-speed running, sprinting, jumping, and tackling) [1]. Unfortunately, such movements could not be identified by the 'distance-based' variables used in the present study. Indeed, an increased amount of jumping and landing places additional stress on tendons and may injure the vulnerable junctional zones (i. e., the myotendinous junction and the enthesis). Owing to the limited number of consistent variables returned from each club and the strict inclusion criteria in the present study, we were unable to quantify the amount of jumping and landing. Therefore, at present it is unclear if differential training stimuli result in a unique physiological response for each tissue type, subsequently influencing the types of non-contact injury sustained by players. This still remains an important question which will require further attention in future research. To do this, investigating other TL variables that might be able to capture the 'uncontrolled nature' of soccer training is warranted. The inclusion of accelerometer data

might be able to provide a more complete picture of the different degrees of mechanical load associated with different movements players experience during training and match play [51]. Indeed, considering the diverse physiological responses on bone, muscle, tendon, and ligament tissue following different intensities of exercise [50], it is possible that a more detailed description of the overall mechanical and physiological load could show differences in the training stresses prior to different types of injury [51].

Previous authors have suggested that an ACWR 'sweet spot' exists (around 0.85-1.35), which could reduce the likelihood of injury and provide a positive training stimulus to prevent injury [53]. This is supported by Colby et al. [21], who noted that players with a 'moderate' ACWR for sprint distance had a lower injury risk when compared to players who experienced 'extremely low' and 'extremely high' sprint ACWRs. This suggests that a rapid increase in sprinting within a short time period should be avoided to reduce the likelihood of muscle injuries [11, 18]. This concept was also recently supported by Jaspers et al. [27], who note a lower injury risk was found for ACWR values between 1.00 and 1.25 in professional soccer players. The authors also noted beneficial effects for medium ACWRs, showing a decreased injury risk in the subsequent week. This is in line with earlier research in different team sports suggesting that a gradual increase of sprint-based activity over time is likely to have a preventative effect on muscle injuries [12]. These observations were, however, not supported within the current study. Conversely, almost all 142 non-contact injuries occurred within the suggested 'sweet spot' zone [53]. This highlights that injuries in the current population occur regardless of the fluctuation in the workload experienced in the weeks preceding injury. Collectively, this further underlines the complexity of risk factors associated with injury as previously highlighted by Windt and Gabbett [10, 54]. The authors highlight both internal (e.g., current fitness status, the player's unique anatomy) and external risk factors (e.g., the playing surface or footwear/equipment used) interact and ultimately result in an inciting event. In addition, although not discussed by Windt et al., genetic predisposition [55], muscle

► Table 3 Accumulated weekly workload data for injury tissue type and relationship with severity.

Workload Variable	Mana LCD	95% Confidence Interval		Min		D	One-Way ANOVA		Correlation	
	Mean ± SD	(lower – up	per)	Min	Max	Range	F	Р	Pearson	Sig.
ACC TD Wk 1										
Muscle	26837±8818	24794	28 880	4452	48 860	44408			-0.065	0.474
Ligament	23483±4427	21124	25 843	17311	33 127	15817	0.881	0.417		
Tendon	24240±8016	21069	27 411	8 5 5 4	37 452	28898				
ACC TD Wk 2										
Muscle	52 124 ± 12 496	49 229	55019	20944	84692	63749			-0.047	0.60
Ligament	45 331 ± 9 585	40 223	50438	26490	58 996	32506	1.038	0.357		
Tendon	50727±13423	45 417	56037	26314	74802	48488				
ACC TD Wk 3										
Muscle	76 320 ± 15 704	72 682	79959	34278	112768	78 491				
Ligament	69 165 ± 13 863	61 778	76 553	51389	91024	39635	0.706	0.495	-0.009	0.92
Tendon	74 395 ± 18 406	67 114	81676	37 020	1 00 297	63 278				
ACC TD Wk 4										
Muscle	101072±18656	96 750	1 05 394	57 936	140670	82734				
Ligament	95 071 ± 19 990	84 420	1 05 723	52 067	1 27 476	75 409	0.311	0.734	0.014	0.881
Tendon	96559±24174	86 996	1 06 122	45 788	1 32 093	86 305	1			
ACC HSD Wk 1								1		
Muscle	1179±560	1050	1309	31	2679	2 648		0.898	0	0.997
Ligament	1127±469	878	1377	502	2 2 9 3	1 791	0.107			
Tendon	1139±482	948	1330	330	1841	1512				
ACC HSD Wk 2										
Muscle	2431±891	2225	2638	482	4609	4127	0.167	0.846	-0.002	
Ligament	2256±1096	1672	2840	1021	4807	3 786				0.98
Tendon	2322±891	1969	2674	699	3993	3 293				
ACC HSD Wk 3										
Muscle	3 563 ± 1 103	3 3 0 8	3819	1 258	6592	5334				
Ligament	3143±1281	2461	3825	1664	6214	4550	0.715	0.491	-0.113	0.211
Tendon	3514±1423	2951	4077	802	5780	4978	- ""			
ACC HSD Wk 4	331121123	2331	1077	002	3700	1370				
Muscle	4729±1346	4417	5041	1842	7706	5 8 6 4				
Ligament	4188±1516	3381	4996	2110	7 266	5 156	0.816	0.445	-0.061	0.500
Tendon	4613±1975	3832	5394	1 294	7 5 7 0	6276	- 0.010			
ACC SPR Wk 1	4013±1373	3032	3334	1234	7 37 0	0270				
Muscle	247 ± 195	201	292	0	965	965				
	247 ± 193 246 ± 155	164	329	41	552	512	0.017	0.983	-0.84	0.35
Ligament Tendon	234±161	170	297	0	743	743	- 0.017			
ACC SPR Wk 2	234±101	170	297	U	743	743				
	474 + 200	407	E 41	2	1214	1212		+		
Muscle	474±289	407	541	2	1314	1312	0.245	0.709	0.100	0.03
Ligament	512±414	291	732	71	1437	1366	0.345		-0.186	0.038
Tendon	509 ± 258	407	611	23	1 068	1 045		+		
ACC SPR Wk 3	605 : 365	606	70.		170-	1.553		+		_
Muscle	695±385	606	784	43	1705	1662	-	0.783	-0.094	0.30
Ligament 	707 ± 508	436	977	193	1757	1 564	0.246			
Tendon	740±426	571	908	23	1 693	1 670				
ACC SPR Wk 4								1		
Muscle	930 ± 504	813	1047	106	2572	2 466	4		-0.001	
Ligament	905 ± 548	613	1197	261	2071	1811	0.107	0.899		0.992
Tendon	953 ± 549	736	1170	92	2437	2 344				

**Abbreviations:** ACC, accumulated workload; TD, total distance; HSD, high-speed distance; SPR, sprint distance; C, coupled; UC, uncoupled; Wk, number of accumulated weeks of workload data.

soreness [56], sleep quality [57], muscle architecture [58], and other stressors associated with competing at the elite level are also likely to affect an individual's injury risk and warrant further attention.

Severe injuries remove players from match play for lengthy durations, often resulting in significant psychological distress for the athlete [59] and a reduction in the teams' performance [60] whilst also having financial implications for professional teams [6]. It is, therefore, important that we aim to understand if the severity of injury may share an association with the workload undertaken by soccer players. However, few studies conducted to date have investigated the relationship between workload and the severity of injury [16, 17, 23, 31, 32]. These previous studies have reported the severity of injury in one of 4 categories (minimal, mild, moderate, and severe) associated with the number of days missed from training and/or games. However, categorising the injury severity in this way limits researchers ability to study the effect of workload on injury severity. Therefore, the present study reported the absolute number of days missed from training/match play. Using this approach, our results indicated that none of the ACWRs or accumulated weekly loads for TD, HSD, or SPR distance was associated with the severity of injury. This finding suggests that workload distance-based data, although important to monitor in a practical sense, has no associative value for the number of days a player will miss following injury. Even though the present study did not find any association, it is important that future research attempts to understand how training load interacts with other individual factors such as fitness level using advanced statistical techniques [54, 61]. Although appreciating cause and effect is important, understanding the mechanisms which influence the individual and the outcome are vital if we intend to reduce the injury burden currently evident within professional soccer.

#### Conclusion

The present study is the first to investigate non-contact injury tissue type and injury severity in professional soccer players using a range of ACWR methods and weekly accumulated workloads. Regardless of the ACWR method used or weekly accumulated workloads, there was no observed differences in workload variables and each injury tissue type. In addition, there was no relationship found between workload variables and injury severity. The current findings reinforce that distance-based workload variables (i. e., TD, HSD, SPR) may not be sensitive enough to differentiate between different injury tissue types. Therefore, the use of ACWRs in isolation should, be acknowledged as a limited approach. As the physiological and biomechanical load-adaptation pathways have diverse response rates, there appears to be a need for studies to investigate the role of different degrees of physiological and biomechanical training load on different tissue types. Moreover, considering the physiological and psychological response to each training exposure in the context of the players' current fitness level and mental condition could allow us to gain more insight into why players get injured. Findings from such research is likely to have implications for the planning of training to prevent injury.

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#### Conflict of Interest

The authors declare that they have no conflict of interest.

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